

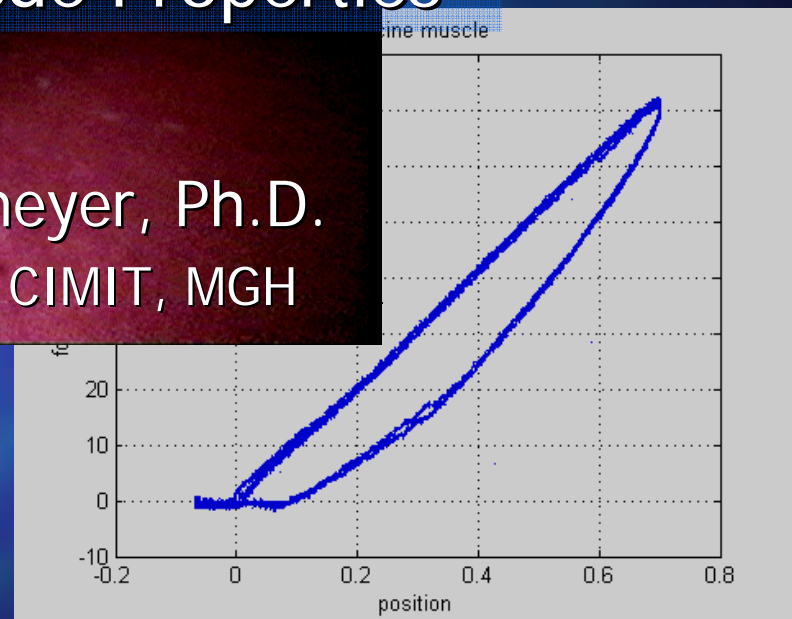


# Does Your Virtual Liver Feel Like Concrete?

(Mostly) In Vivo Techniques for  
Measuring Soft Tissue Properties



Mark P. Ottensmeyer, Ph.D.  
Simulation Group, CIMIT, MGH



# IPAM mini-review

- Satava
  - sims good enough to allow mistakes
  - digital libraries of patient specific cases (from Virtopsy)
- Teran/Oliker/Cutting
  - fast FE, spring-mass models for plastic surgery
  - deformation & cutting
- Terzopoulos
  - facial tissues, neck/body muscles
- Schill
  - ophthalmic surg sim – deformation & tearing
- Meglan
  - generalizability, “provenance”
  - Top-down face validity requires redo for each new sim
  
- Soft tissue model material parameters – how do you get them?



- Tissue properties - a black hole

Satava, c. 2001

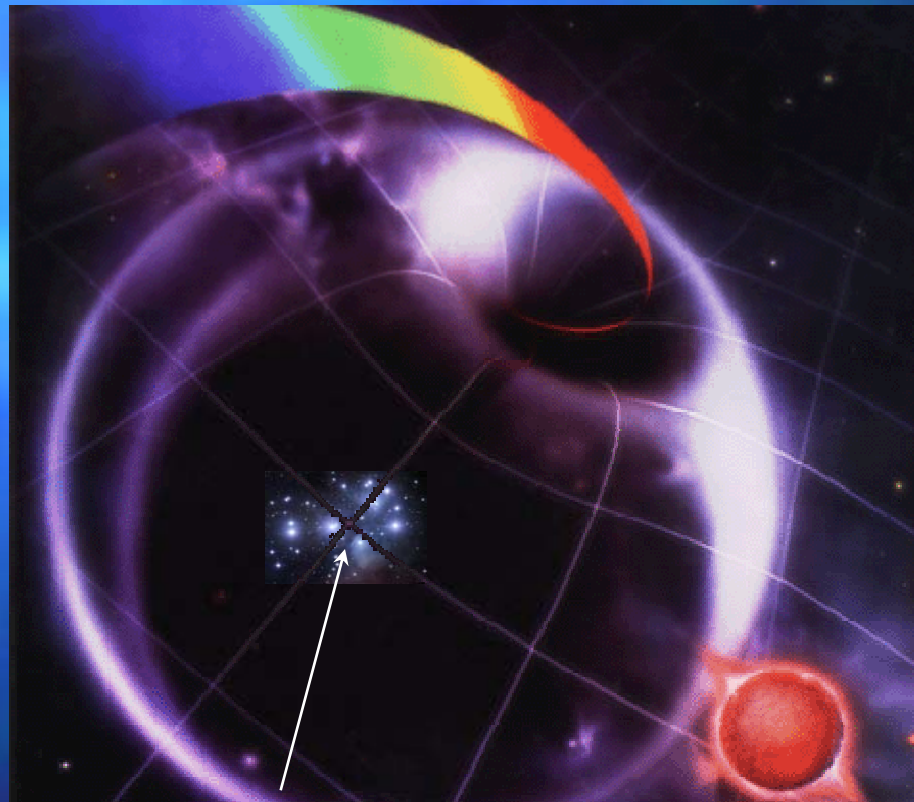


image: National Geographic Picture Atlas of Our Universe, 2<sup>nd</sup> ed., 1986

c. 2008: Harders, De, Ottensmeyer & friends!

11 January 2008

Scientific Computing Applications in  
Surgical Simulation of Soft Tissues



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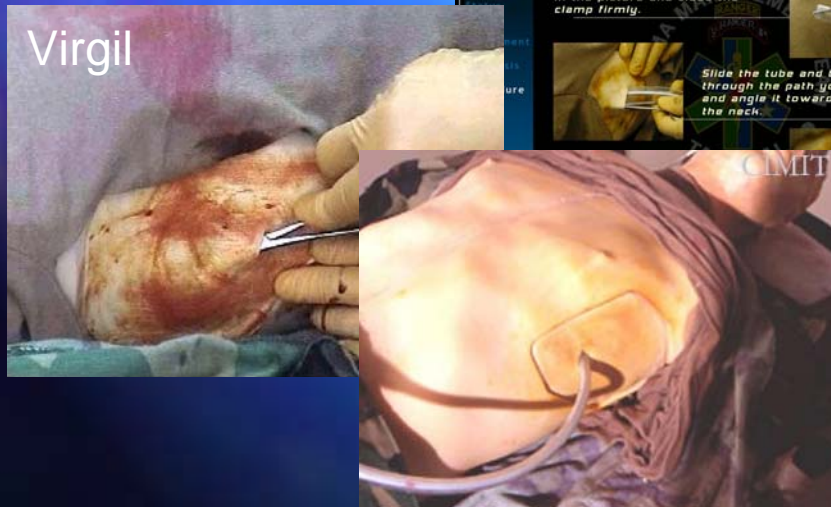
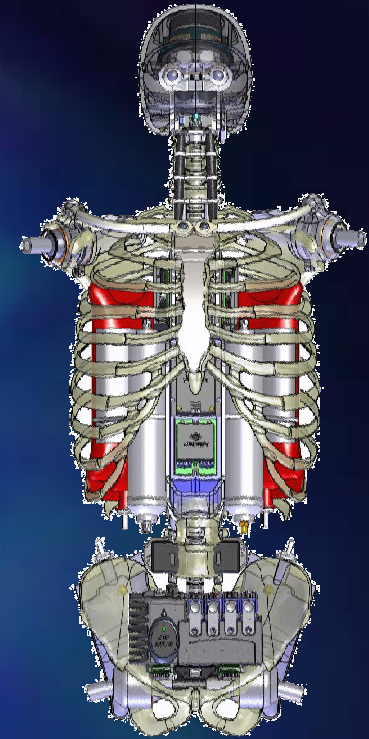


- MGH/CIMIT Simulation Group

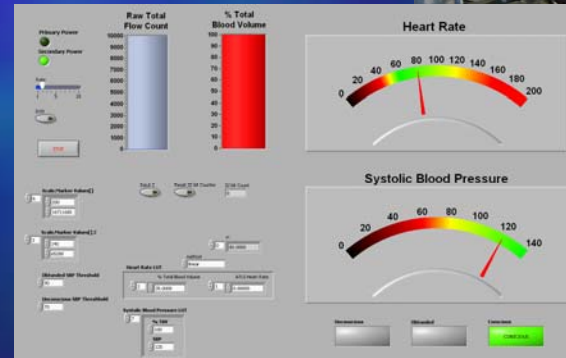
- basic science and proof-of-concept systems for medical training through simulation

- Multi-disciplinary research team

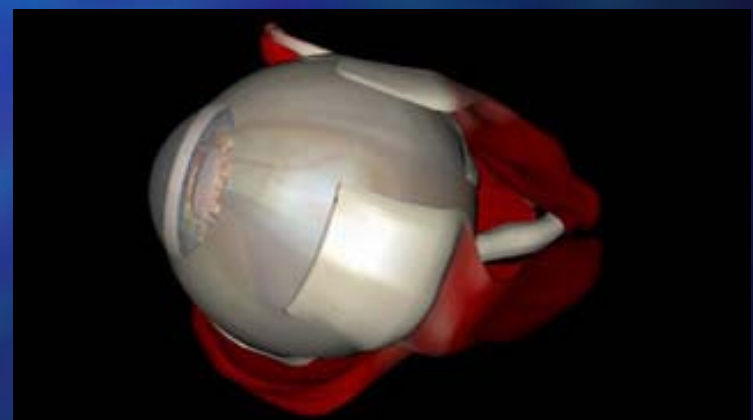
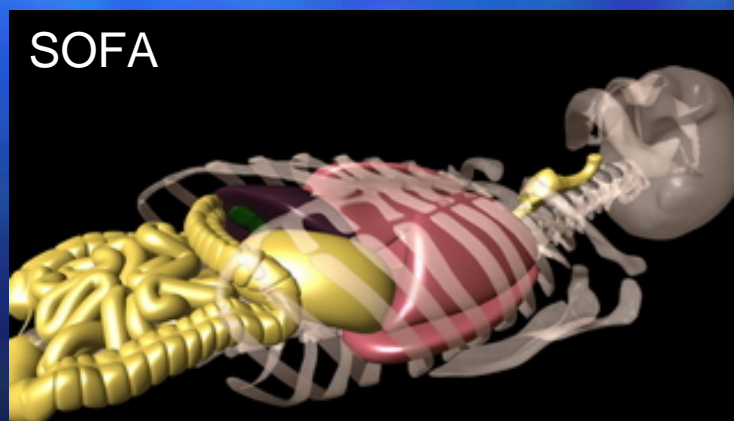
- M.D. (radiology), mech. eng., comp.sci., industrial designer, fine arts



### COMETS

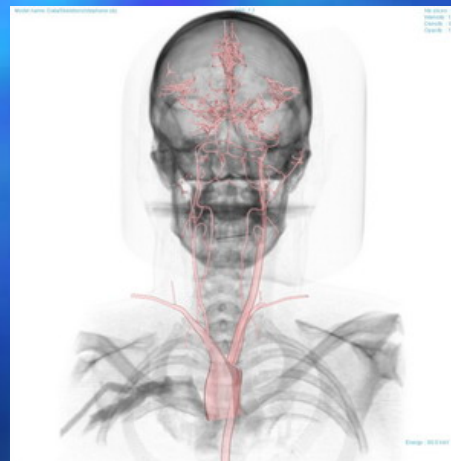
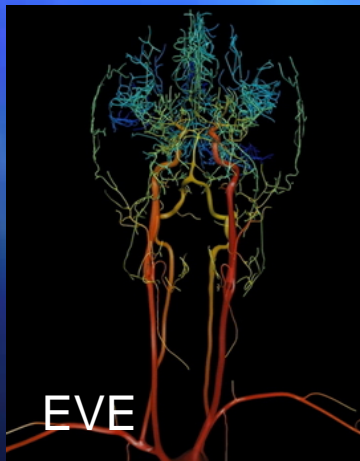


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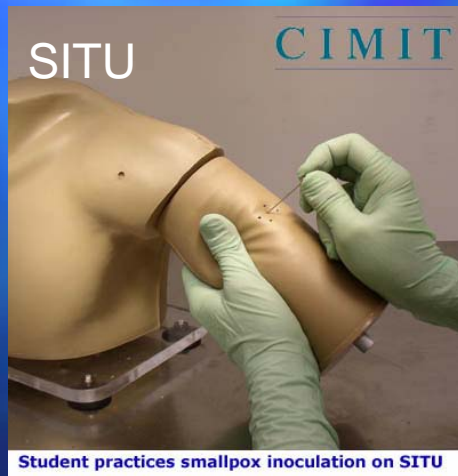




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# Outline

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- *in vivo* tissue testing techniques & devices
  - taxonomy axes?
  - compliance testers
  - elastographic techniques
  - briefly cutting/piercing
  - applications sprinkled in
- summary & a few extra slides

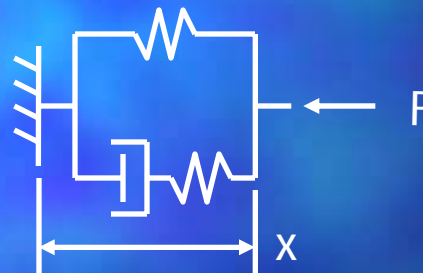
# Possible tissue testing taxonomies

- Measurement interaction technique
  - Tension, compression, indentation, shear, aspiration
  - Puncture, cutting (single blade/scissors), crushing, fracture
  - Non-contact, non-invasive
- Rate/range of interaction
  - Static/quasi-static (ignoring viscosity)
  - Manual manipulation rates (2Hz or less)
  - Soft impact, moderate frequency (<300Hz)\*
  - High speed impact, ultrasound response
  - Strain level: linear to non-linear material and geometric domain
- Tissue type
  - Solid organ (liver, kidney, brain, muscle...)
  - Hollow organ (intestine, stomach, bladder, vessels...)
  - Structural (bone, cartilage, tendon, ligament...)
  - Others?
- Application
  - Surgical simulation (real-time & JND constraints)
  - Tissue engineering, implants, prosthetics (offline models?)
  - Physiology simulation (voice production – here's the \*)
  - Body armor development (model impactor + armor + underlying tissue)



# Living Tissues

- Material properties/behaviors
  - visco-elasticity—standard linear (Kelvin) model



- Prefer geom.-indep. properties, *not* spring consts.
- Non-linear, *poro*-visco-elastic, anisotropic, inhomogeneous, age/temp/pathology-dependent
- Independent experiments for each parameter!
- Yamada ('70), Duck ('90), others: *in vitro*

# Living Tissues

- Measurement complications
  - Invasiveness of testing—surgical access to organs
  - Motion corrupts data: cardiac, pulmonary action
  - Limited testing periods
  - Non-ideal tissue “samples”: no standard shapes
  - Tensile tests difficult
  - Humidity, temp., body fluids—effects on hardware
  - *Human testing protocol approval!*
  - ...



# Measurement Techniques

- Compliance testing
  - Deform tissue locally, measure “ $F(t)$  vs.  $X(t)$ ”
  - Use simple approximation or iterative FEA to extract parameters
- Elastographic testing
  - Image strain field (2-D, 3-D), motion amplitude
  - Invert to generate qualitative elastograms
  - Iterate on inverse problem for quantitative
- Cutting & needle insertion
  - Recording  $F(t)$  vs.  $X(t)$
  - Separate elastic, fracture, frictional components
  - Currently instrument-specific

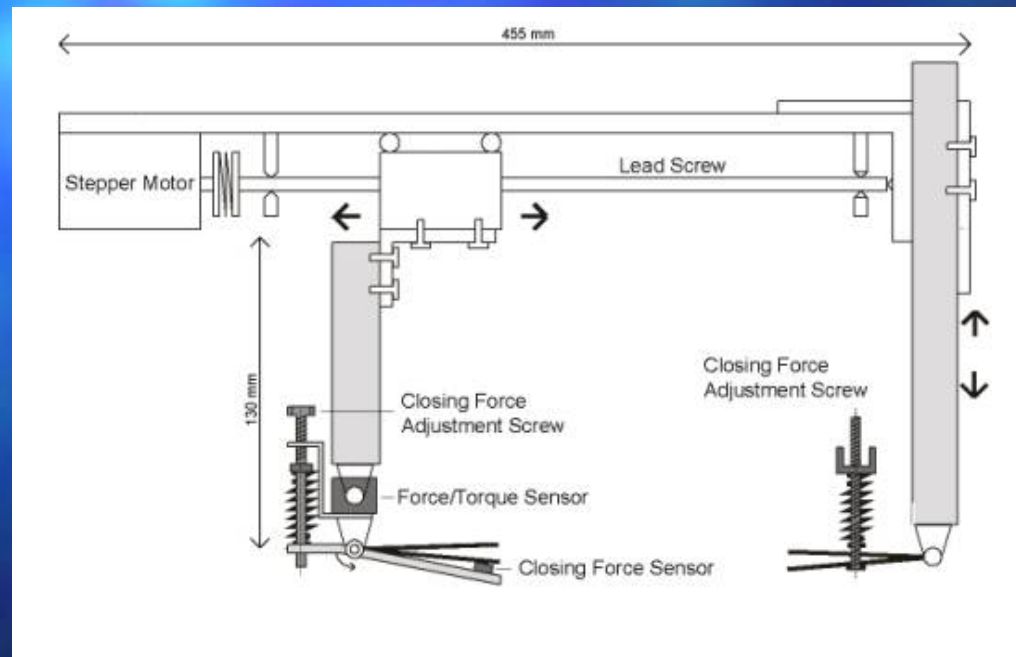
# Compliance techniques

- Deformation modes
  - tension
  - compression
  - indentation
    - side trip into bench top "life support"
  - torsion (shear)
  - aspiration/suction



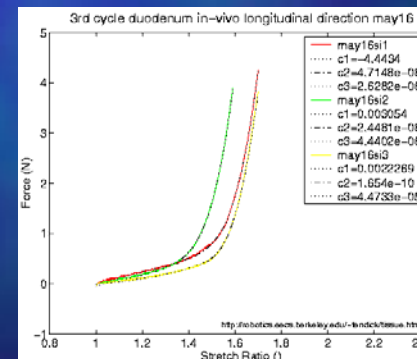
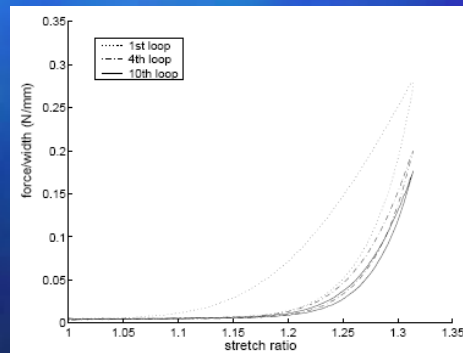
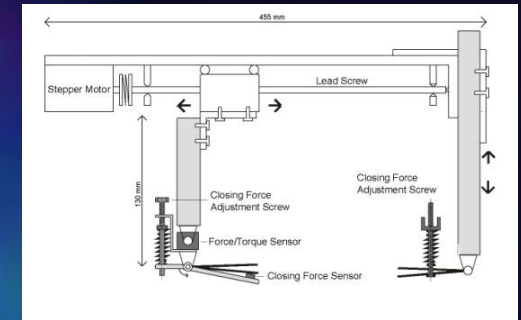
# Compliance: tensile testing

- Tendick, et al.; UCSF/Berkeley
  - GiPSi: open source framework for surgical simulation
  - Enhanced perception for soft tissue manipulation
  - Interactive-rate FEM techniques
  - Creation of tissue property “atlas”



# Compliance: tensile testing

- Uniaxial tensile testing apparatus
  - Babcock graspers; open abdomen
  - in vivo/vitro porcine stomach, sm. bowel, gall bladder (Brower et al., MMVR01)
  - 40Hz control/sampling; >150mm motion; 0-6N applied
- Curve fitting
  - $F(\lambda) = \alpha e^{\beta\lambda}$ ;  $\lambda = l/l_0$
  - Tests include response to pre-conditioning: large for in vitro
  - online resource for force-stretch ratio data



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# Compliance: compression tests

- BioRobotics Lab, U. Washington
  - Hannaford, Rosen, et al.
  - Understanding surgical gestures, force/position range
    - Blue Dragon, Red Dragon, Markov model description
  - Improving tactile feedback for MIS
  - Supporting surgical simulation community



<http://brl.ee.washington.edu>

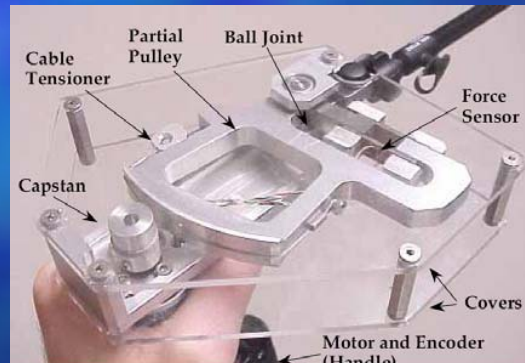


# Compliance: compression tests

- Motorized Endoscopic Grasper
  - Babcock grasper, MIS (10mm port), usually open laparotomy
  - *in vivo* porcine solid & hollow organs
  - improved haptic tissue discrimination; characterize tissue *in vivo vs. post mortem*
  - testing up to 3Hz; 30mm RoM; 25N (70 max) force (surgical scale)



FREG

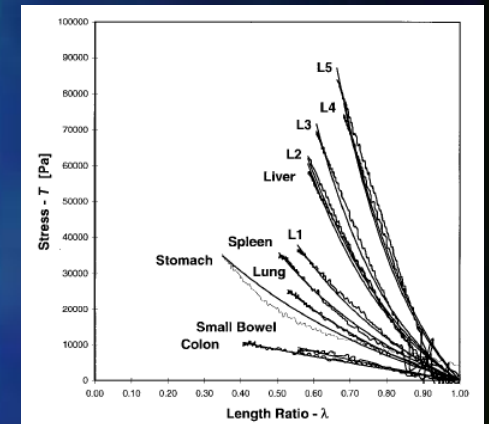
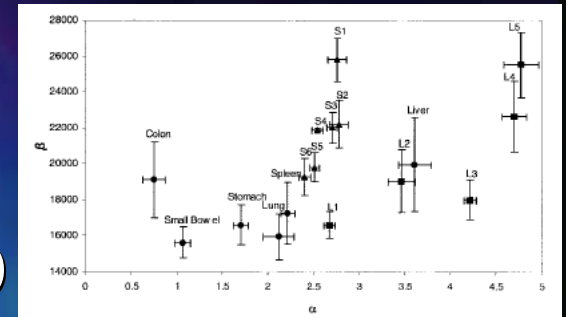


MEG



# FREG/MEG: selected results

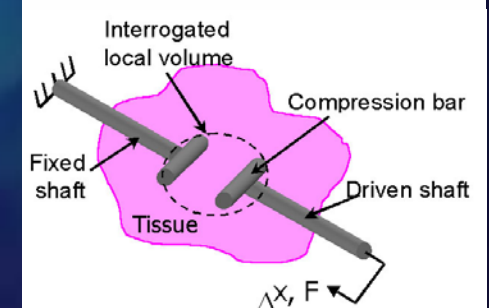
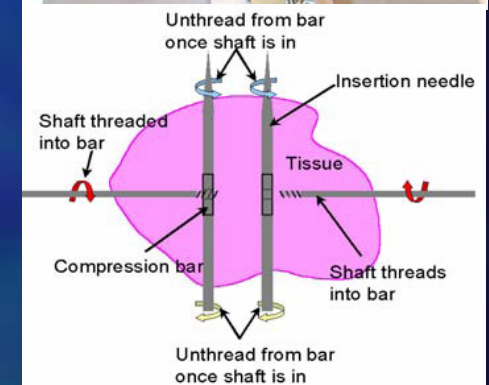
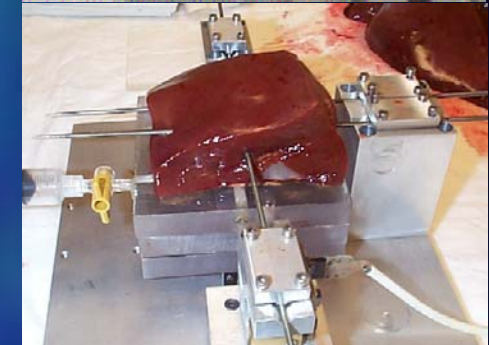
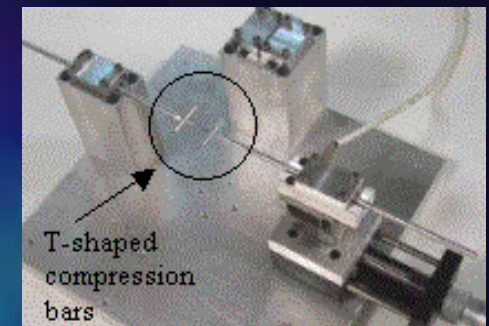
- Tissue stiffness (FREG) (Rosen et al., MMVR98)
  - distinguishable stiffness: *in vivo* porcine liver, spleen, small bowel, colon, stomach, lung
  - Curve fitting:  $\sigma(\lambda) = \beta(1 - e^{-\alpha(1-\lambda)})$ ;  $\sigma = F/A_0$ ;  $\lambda = l/l_0$
- Tissue stiffness (MEG) (Brown et al., MICCAI03)
  - liver/small bowel *in vivo*  $\Rightarrow$  *in situ*  $\Rightarrow$  *ex corpus* (3x)
  - preconditioning, stress relax'n effects differ *post mortem*, changes between *vivo*, *ex corpus* @ 25hrs
- Color change (De et al. MMVR06)
  - MEG compression, Canon Powershot A80, spectrophotometer, subjective validation
- Damage thresholds (De et al., IJRR07)
  - porcine liver (<80kPa @ 30s), ureter (~100kPa), small bowel (~100kPa)
  - H&E (morphology), MPO IHC (inflammation), caspase-3 IHC (apoptosis) staining





# Compliance: compression tests

- BioRobotics Lab, Harvard U.
  - Howe, Kerdok, Maeno, et al.
  - “Enabling Technologies for Advanced Soft Tissue Modeling”
  - Internal parenchymal tester for solid organs
  - Motorized, integrated with NELP system
    - 0-100mm/s, 36% strain (7mm compression)
  - Proof of concept results (Kerdok&Howe’03)
  - QLV model, 3 time constants: 0.102, 1.47, 27.76s



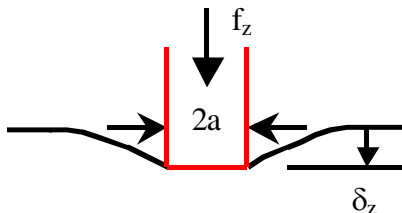
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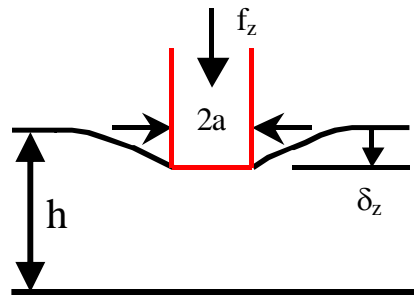


# Compliance: indentation

- Closed form solutions
  - linear, isotropic, homogeneous, semi-infinite
  - normal indentation (frictionless)


$$E_{slip} = \frac{(1-\nu^2) f_z}{2a \delta_z}$$

- Hayes' correction (Hayes et al., J.Biomechs72)
  - correction exists for hemispherical indenter as well

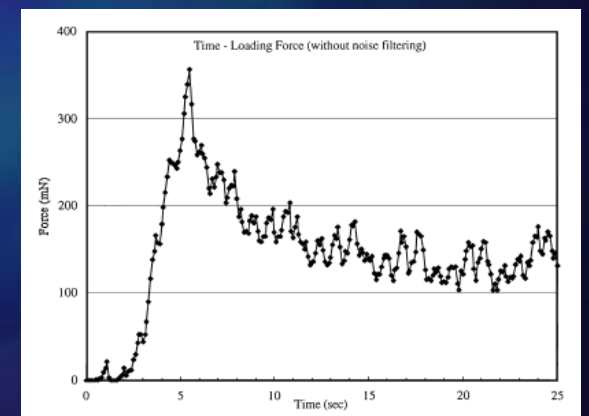
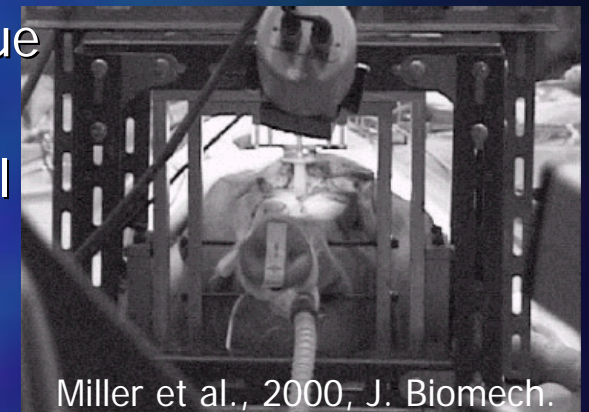
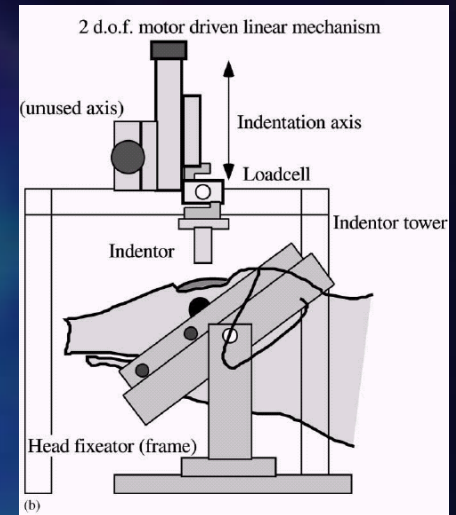

$$E_{slip} = \frac{(1-\nu^2) f_z}{2a \delta_z K \left\{ \frac{a}{h}, \frac{x}{h}, \nu \right\}}$$
$$K = 1.23 + 1.26 \frac{\delta_z}{h}$$

# Compliance: indentation

- Common method for tissue testing *in vivo*
  - Miller, U. Western Australia: porcine brain
  - Carter, U. Dundee, UK: human liver
  - Ottensmeyer, MIT: porcine liver
  - Kerdok, Harvard: porcine liver, spleen
  - Tendick, UCSF; Srinivasan, MIT: porcine abdominal tissues
  - De, RPI: porcine tissues, human cadavers

# Compliance: indentation tests

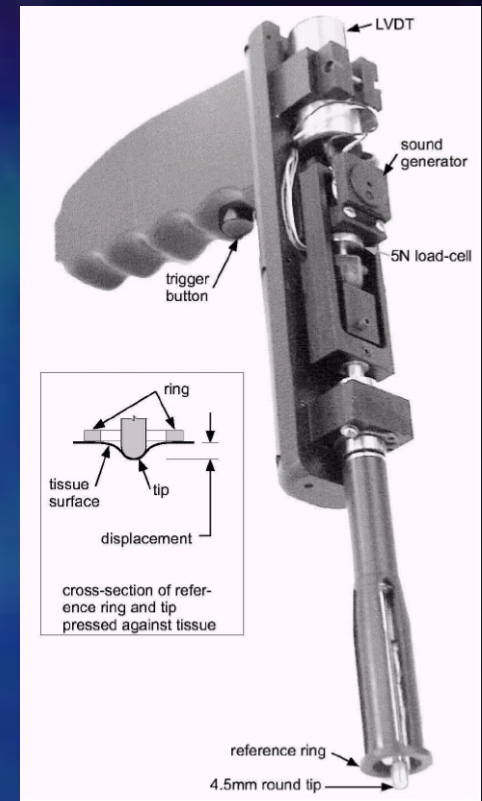
- Intelligent Systems for Medicine Lab; U. Western Australia
  - Miller, et al.
  - non-rigid registration, neurosurgical planning & simulation, predicting injury due to baseball impact
  - porcine brain *in vivo*, 10mm flat cylindrical indenter
  - 1mm/s max V; 3.9mm indentation used; 400mN max (applied *in vivo*)
  - Iterative FEA using hyperviscoelastic constitutive law, MRI for BCs



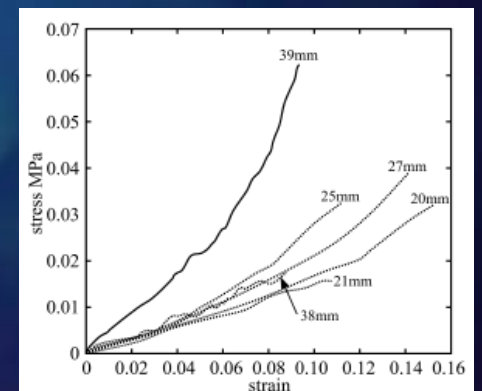


# Compliance: indentation tests

- Surgical Skills Unit, Dundee U., UK
  - Carter, Cuschieri, et al.
  - diagnostics, tool design, surgical simulation
  - manual application: 5mm (10 max) *in vivo*; ~1N (5 max) *in vivo*
  - 4.5mm hemispherical indenter, reference ring 12/18mm ID/OD
  - ***first human liver in vivo!***
  - healthy vs. diseased (cholestatic liver w/bile obstruction: 2x stiffness)
  - porcine liver & spleen *in vitro*

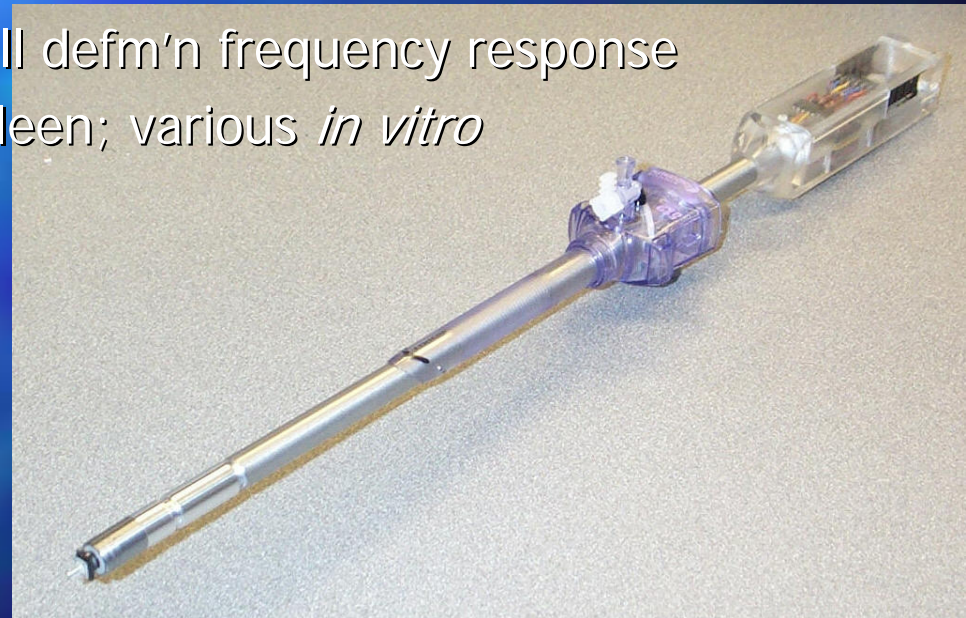


Carter et al., 2001, Med. Imag. Anal.



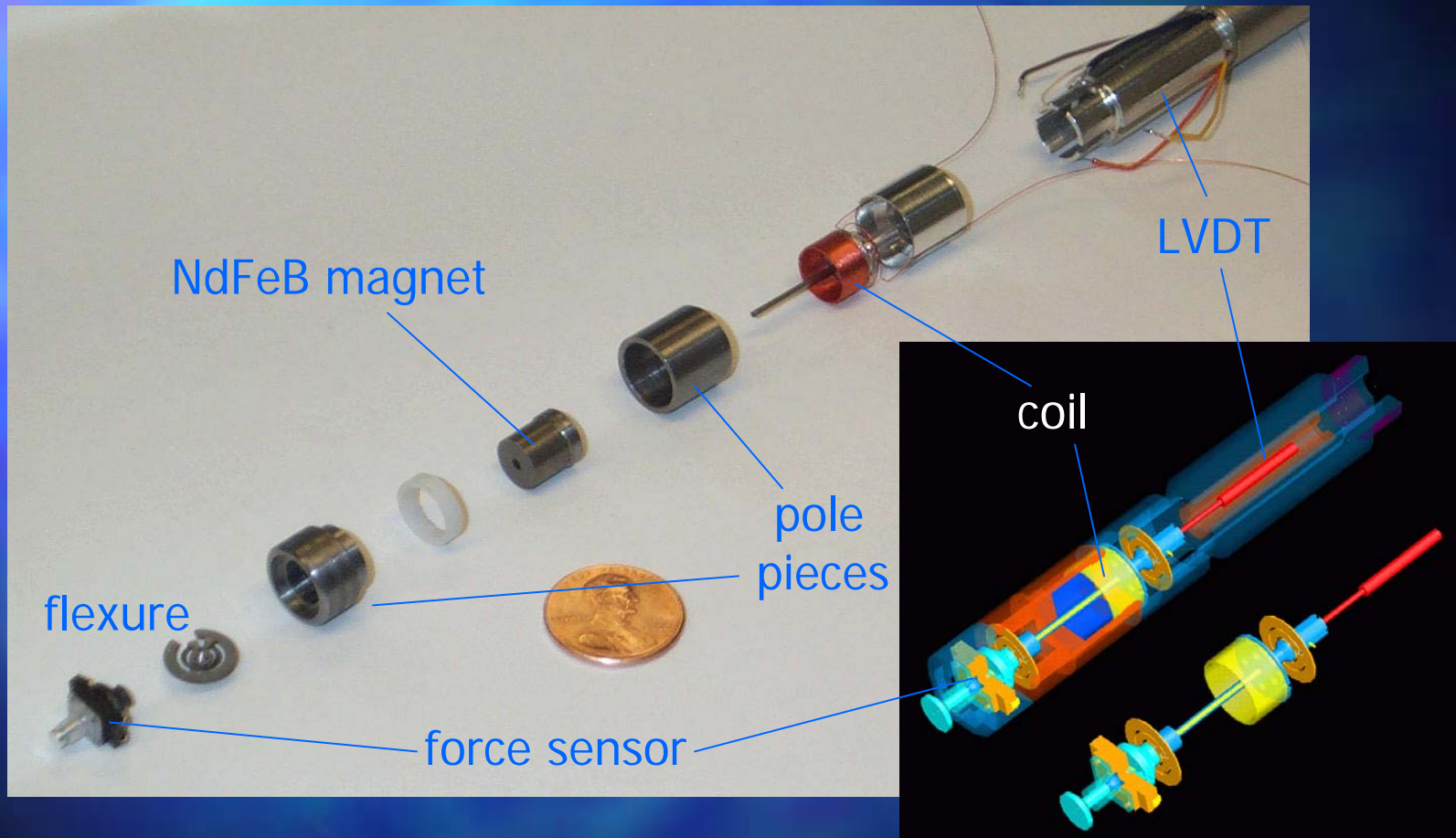
# Compliance: indentation tests

- Haptics Laboratory, MIT
  - Ottensmeyer, Salisbury
  - support for planned laparoscopy simulator
  - minimally invasive; 2kHz sampling; 80Hz resonance; 1mm RoM; 300mN max force; 5mm flat cylindrical indenter, 12mm OD
  - characterization of small defm'n frequency response
  - *in vivo* porcine liver, spleen; various *in vitro*





# TeMPeST detail

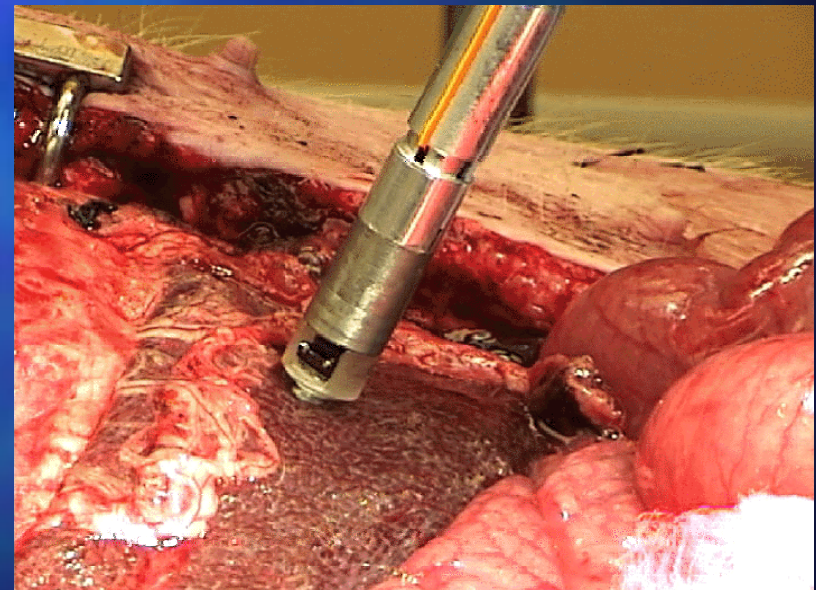
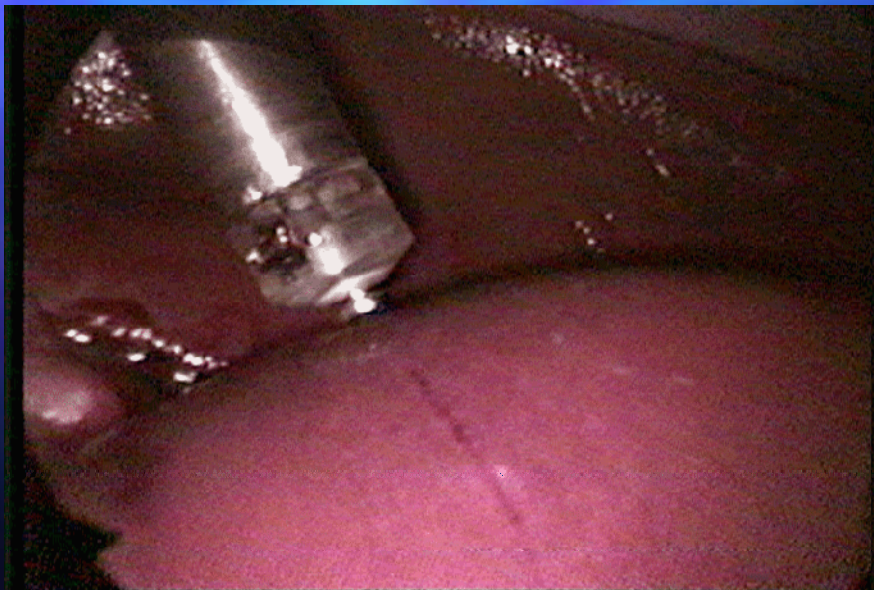
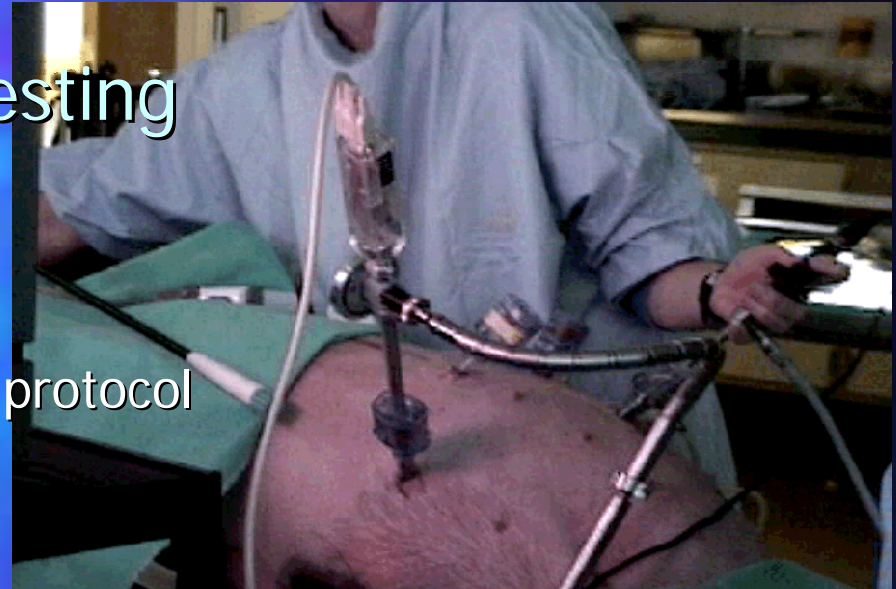




# TeMPeST *in vivo* animal testing

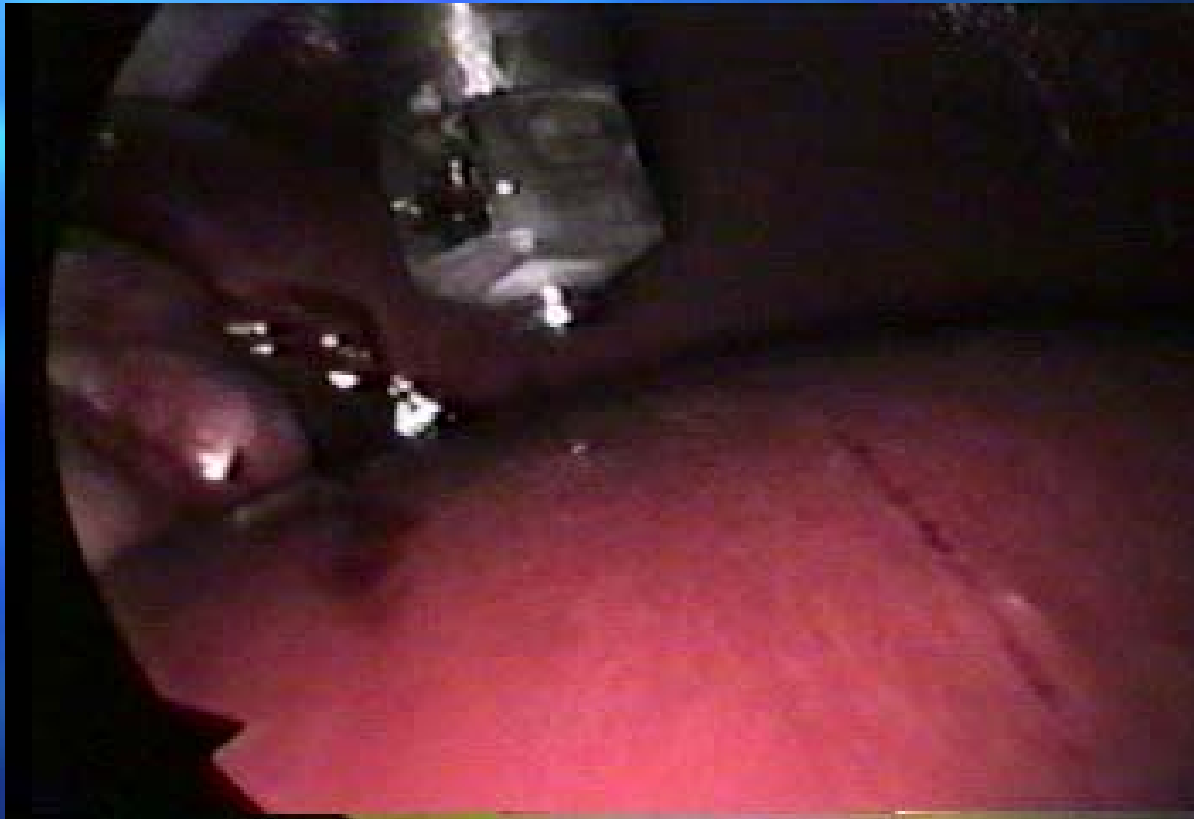
## ■ Details

- ARC (Dartmouth), HCMIS
- pigs in surgical tool testing protocol
- laparoscopic & open
- video clip



# TeMPeST *in vivo* animal testing

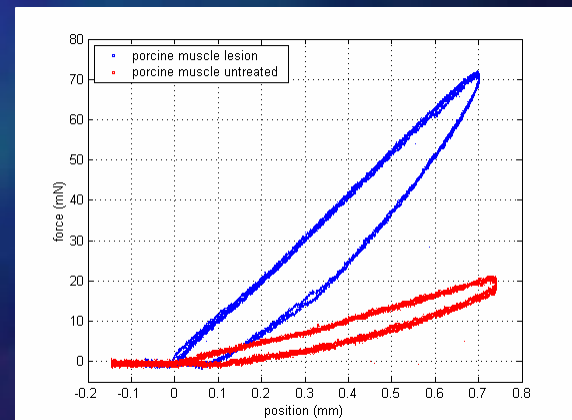
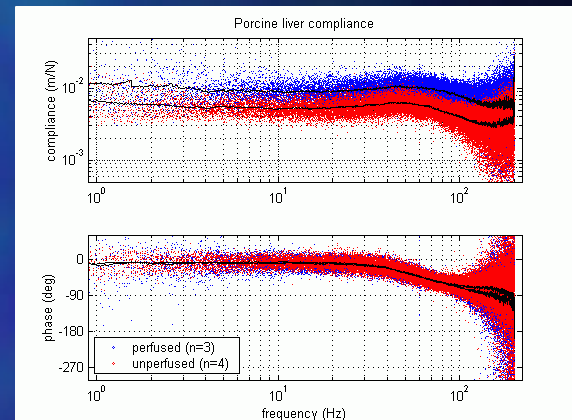
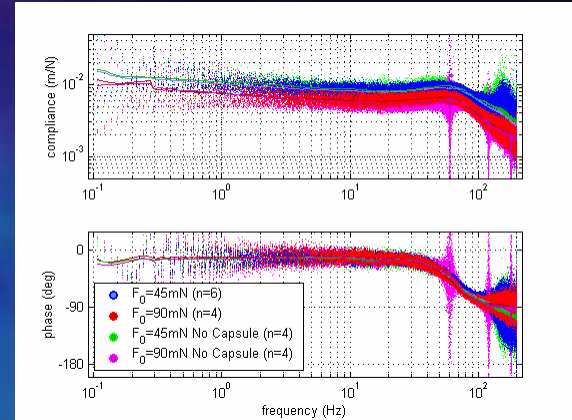
- Typical test sequence





# TeMPeST results

- A few examples...
  - examination of effect of capsule
    - stiffer than underlying parenchyma
  - effect of organ perfusion
    - blood pressure pre-stresses capsule
- porcine muscle
  - quasi-static comparison of normal tissue with HIFU lesion





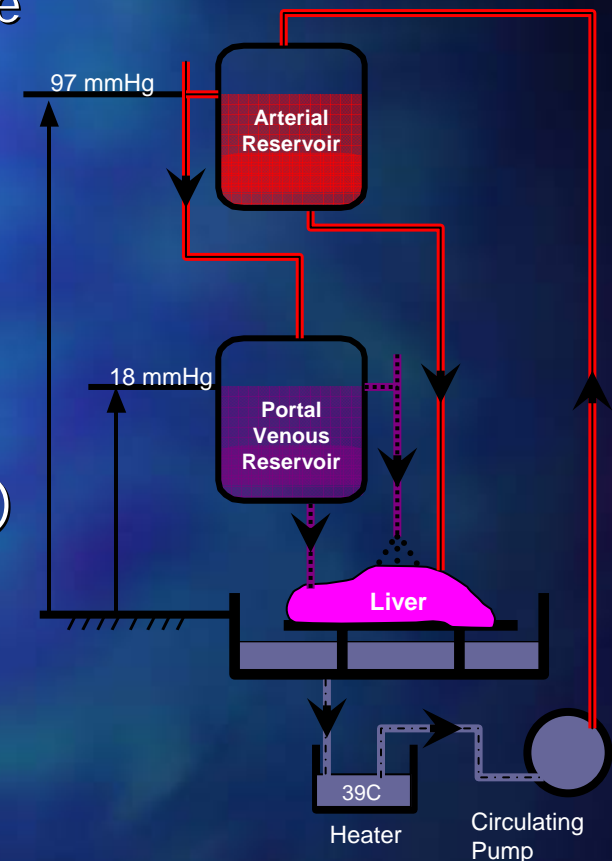
## A short detour...

- *in vivo* “gold standard” subject to limitations
  - time, cardiac/pulmonary action, etc.
- *in vitro* problems
  - coagulation, loss of fluids, change in boundary conditions
- Perfusion
  - inspired by transplant literature, without chilling
- *in vitro* “silver standard”
  - maintain blood pressure (venous, arterial)
  - maintain temperature
  - maintain osmotic, oncotic balance

# Normo-thermic Liver Perfusion System

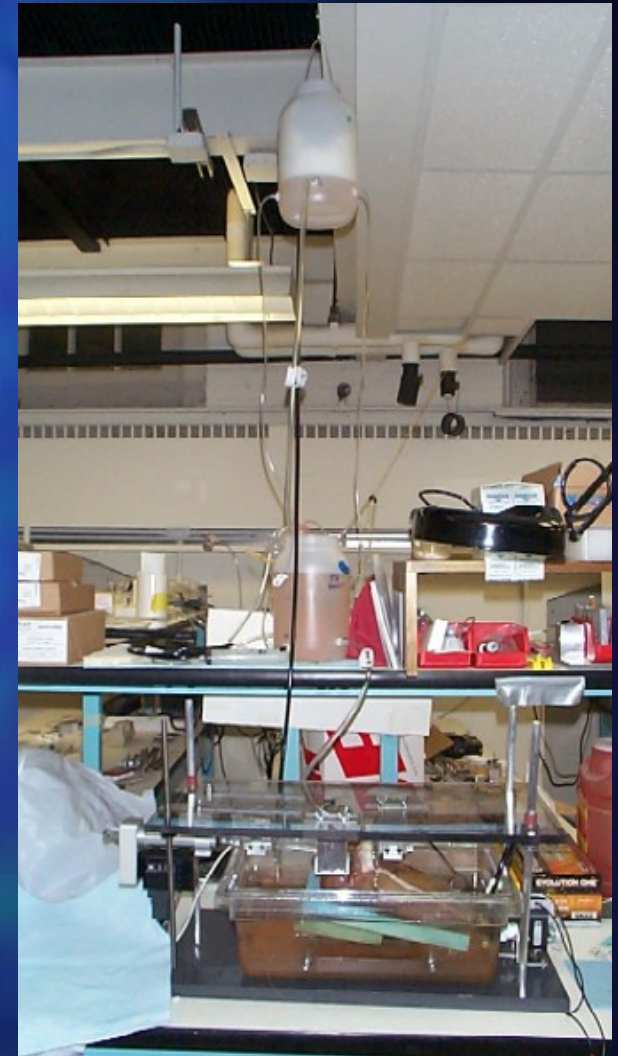
## ■ Perfusion system

- provides physiological solution to whole organ
- for liver: hepatic arterial and venous pressures, drains through portal vein
- physiologic temperature control
- hydration maintained
- Lactated Ringer's w/dextrose, Hetastarch (osmotic & oncotic balance)



# Perfusion Rig

- Initial version
  - hydrostatic supplies of perfusate: high elevation for arterial supply, lower elevation for venous
  - pump, heater below bench

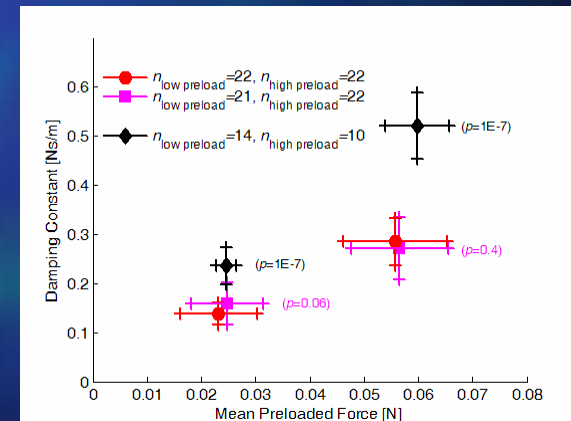
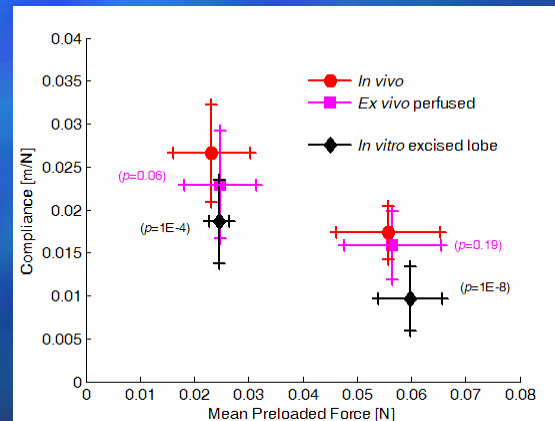
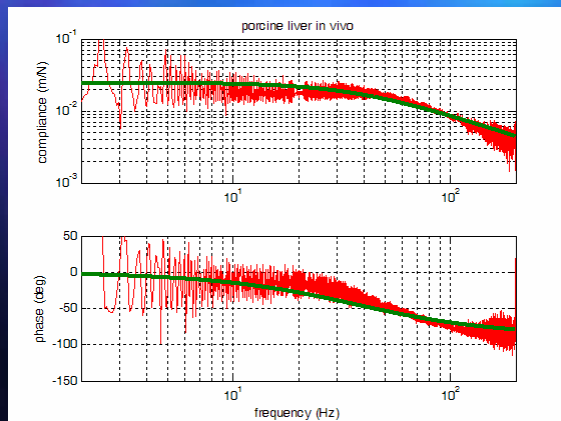
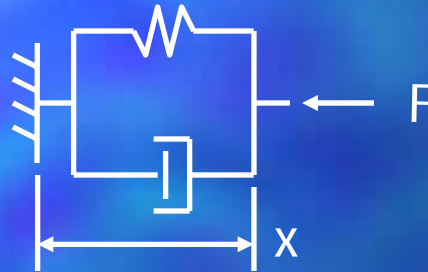




# Perfusion validation

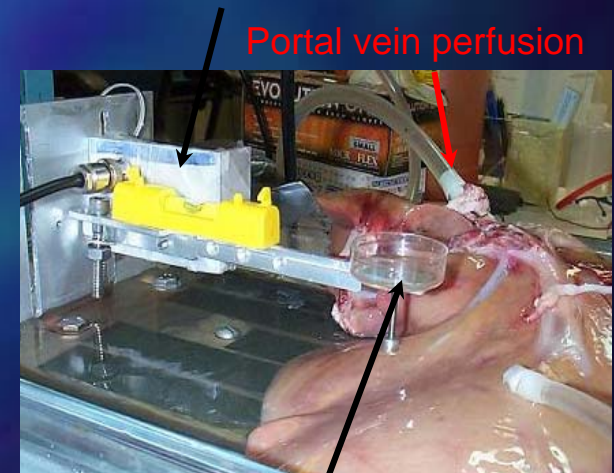
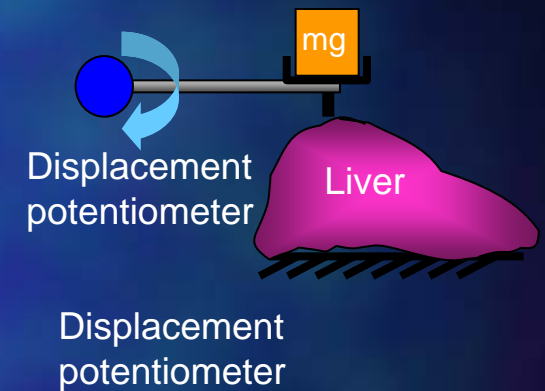
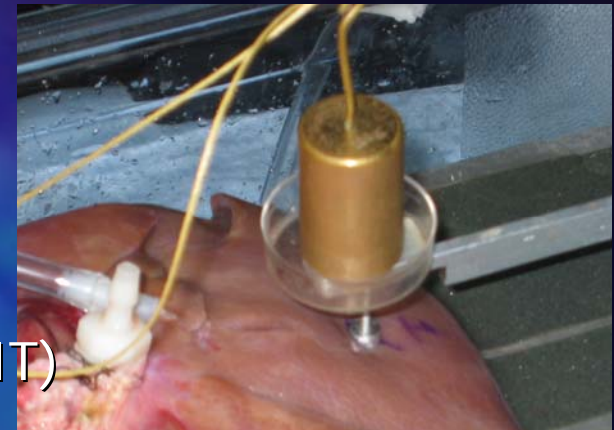
## ■ TeMPeST tests

- compared *in vivo*, perfused, unsupported conditions
- response similar to linear spring-damper
- statistical comparison of stiffness, damping coefficient



# Compliance: indentation

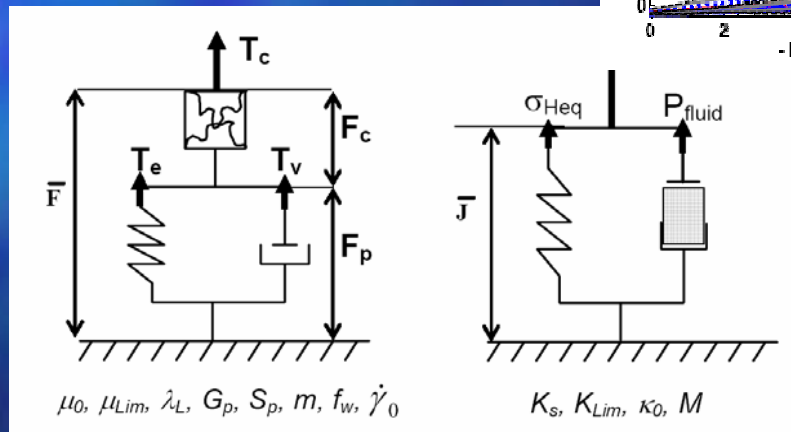
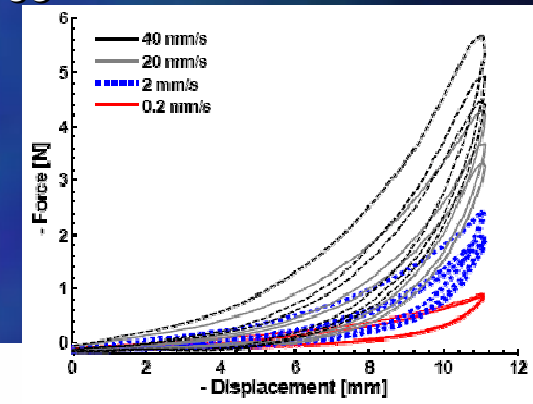
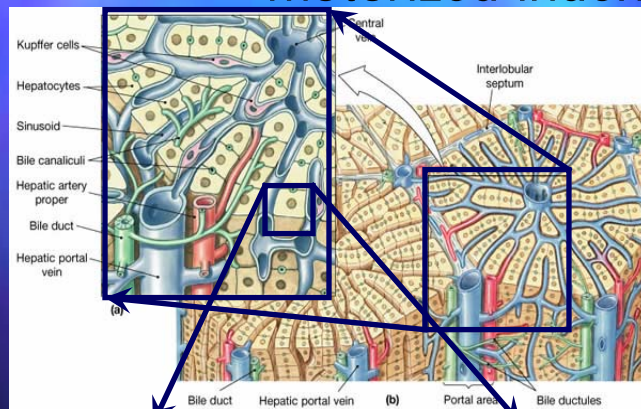
- BioRobotics Lab, Harvard
  - Kerdok, Howe (BRL); Ottensmeyer (CIMIT)
  - large deformation tissue characterization
  - creep characterization, testing *in vivo* vs. perfused *in vitro* vs. unperfused *in vitro*
  - 0.25" flat cylindrical indenter; 1kHz sampling; 10mm RoM; 20/100/200g step load (manually placed); open abdomen
  - porcine liver *in vivo* vs. *in vitro*
  - validated perfusion system for large deformation



Indenter and weight cup

# Compliance: modeling

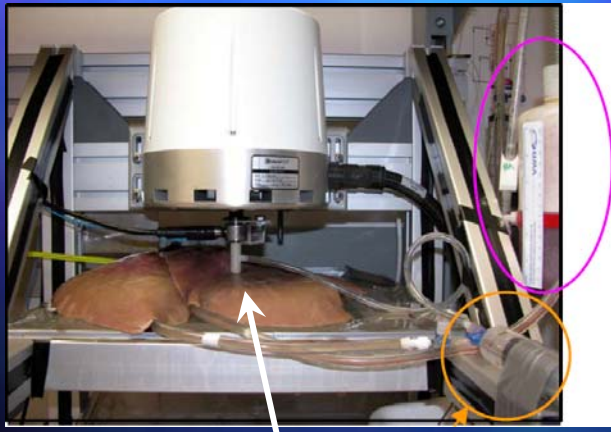
- Improved model
  - liver anatomy suggests more complex model
  - hyperelastic, poro-viscous elements
    - Socrate/Kerdok modification of Arruda-Boyce
  - motorized indenter experiments





# Compliance: indentation

- BioRobotics Lab, Harvard
  - Howe, Kerdok, Jordan
  - ElectroForce TestBench, *in vitro* w/perfusion system; 12mm motion
  - stress relaxation, arbitrary inputs
  - Non-slip suction contact
  - 3-D ultrasound



indenter tip



ultrasound probe



arterial reservoir

venous reservoir

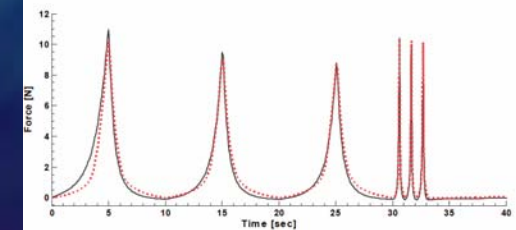
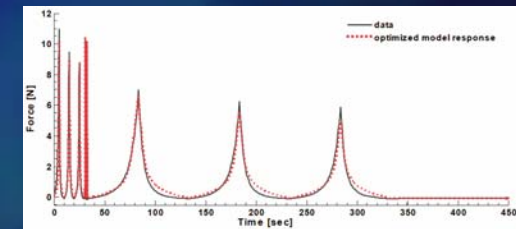
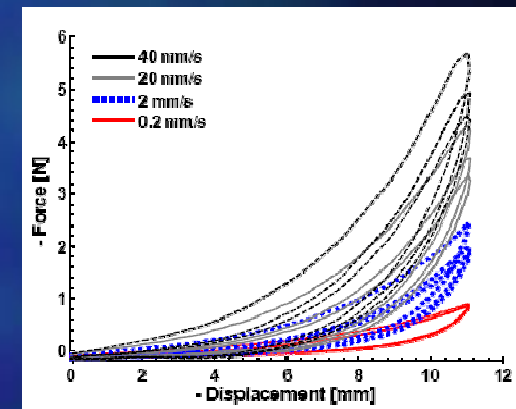
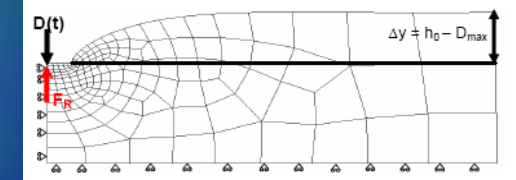
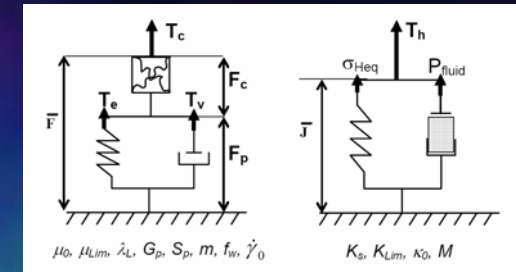
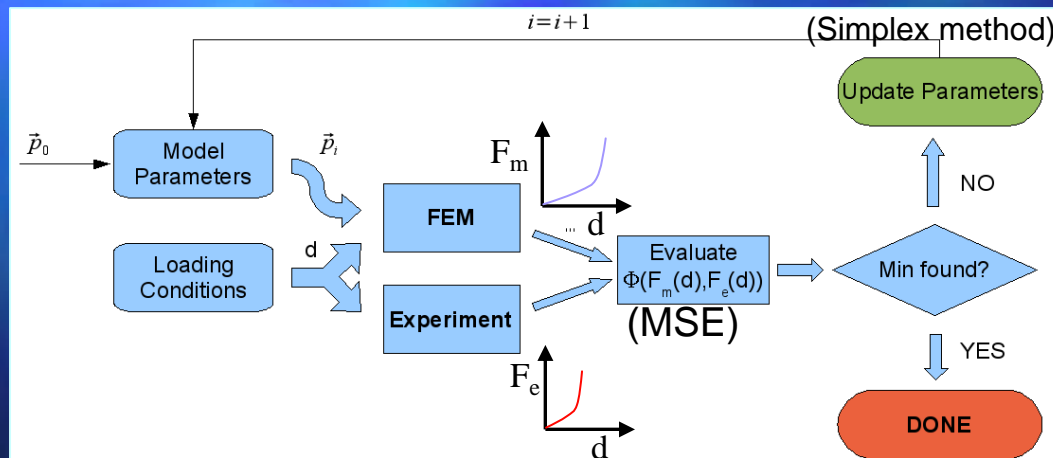
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# Compliance: parameter extraction

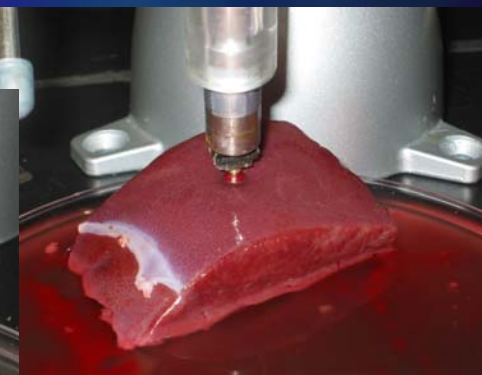
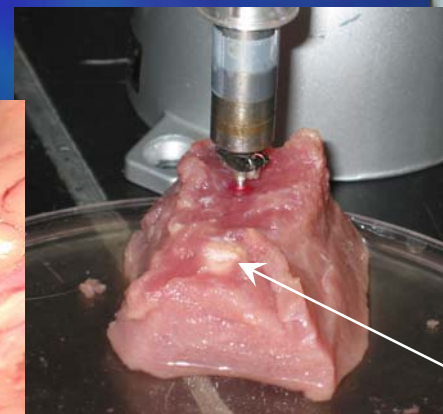
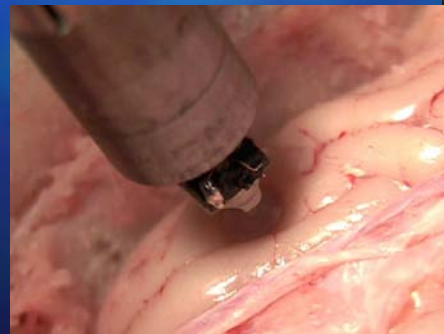
- Parameter identification algorithm
  - iterative FE approach
  - simulate with trial parameters
  - compare with experiment
  - update parameters
  - repeat until convergence





# Compliance: more tissues

- *In vitro* tests
  - Rodent (rat) liver, kidney
    - NASA Ames/Stanford Virtual Rat Project
    - (Bruyns & Ottensmeyer, MICCAI'02)
  - Ovine, bovine, human vocal tissues
    - MGH Ctr. for Laryngeal Surgery & Voice Rehabilitation
    - Testing real tissues to quantify properties to develop compatible biopolymers
  - Porcine brain, muscle/liver
    - In situ cerebral cortex testing
    - Harmonic Motion Imaging (Konofagou et al., Ultrasonics'04)



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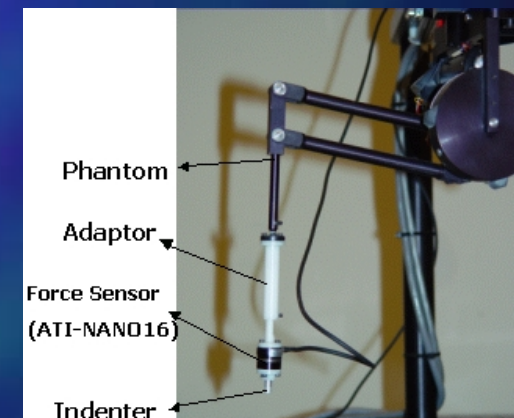
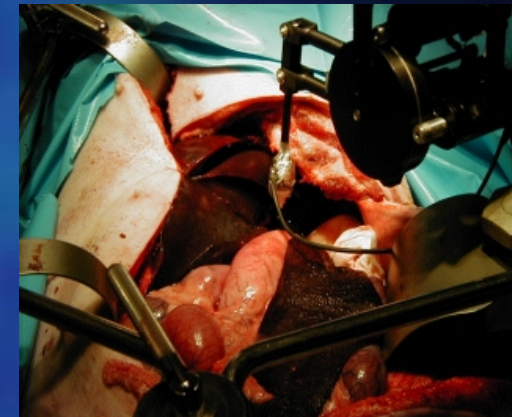
HIFU lesion

38



# Compliance: indentation tests

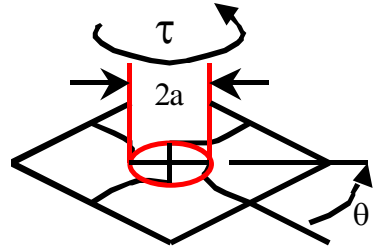
- Phantom 1.5 (SensAble) – a neat little robot!
  - 125Hz mechanical resonance
  - 190x270x380mm workspace
  - 1.4N continuous force (8.5N max)
- Tendick (UCSF/Berkeley)
  - 20mm hemispherical indenter
  - *in vivo* porcine stomach/liver/spleen/skin
  - Brower et al., MMVR'01
- Srinivasan (MIT TouchLab)
  - ramp-hold, sinusoidal (0-3Hz) motion
  - 2mm flat cylindrical indenter
  - *in vivo* porcine liver/spleen/kidney/esophagus
  - Kim et al., MICCAI'03, Tay et al., MMVR'02
- De, et al. (RPI)
  - human cadaver measurements, in press



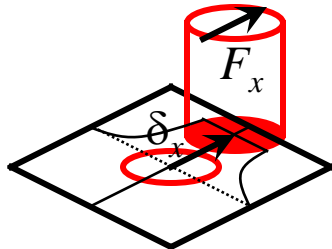
<http://touchlab.mit.edu>

# Compliance: shear tests

- Closed form solutions
  - semi-infinite, non-slip, isotropic, homogeneous, linear
- Torsional shear


$$E = \frac{3(1+\nu)\tau}{8a^3\theta}$$

- Tangential shear


$$E = \frac{(2+\nu+\nu^2)f_x}{2\pi a\delta_x}$$



# Compliance: torsional shear

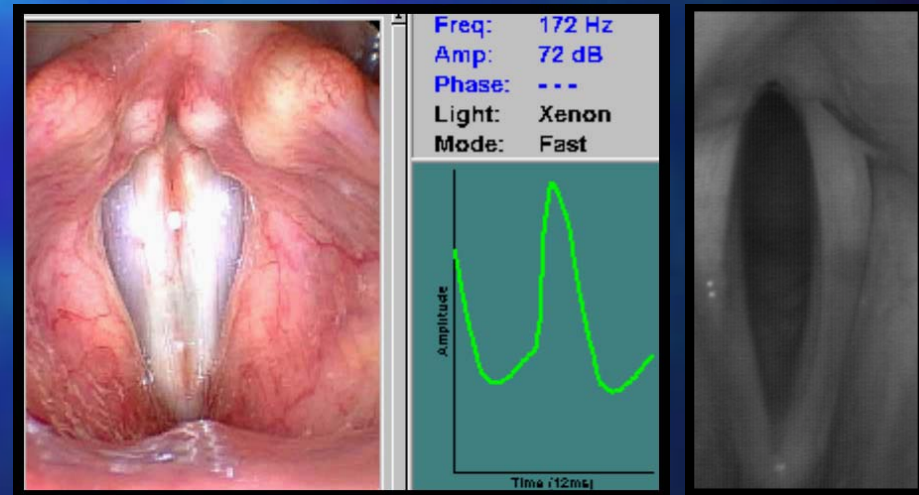
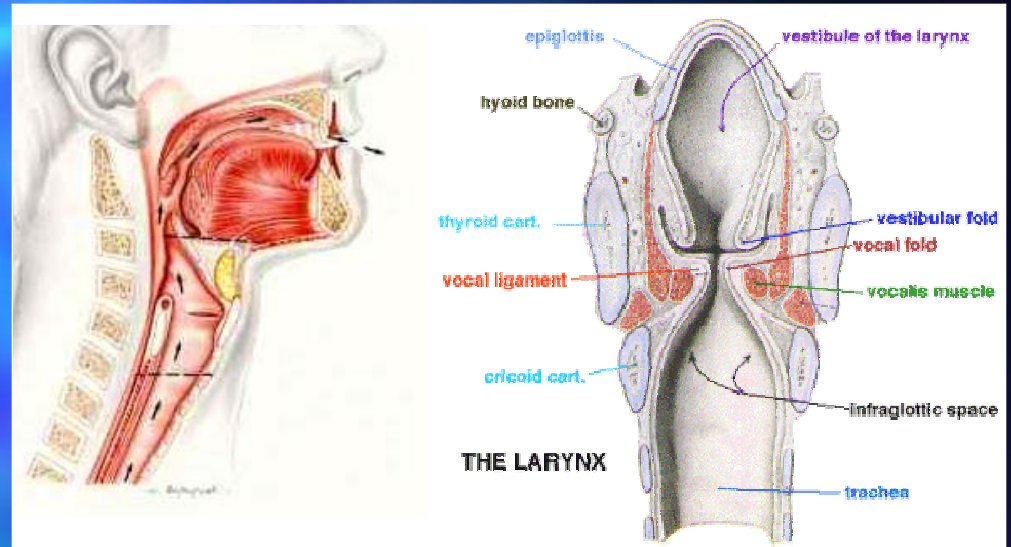
- ROSA2: Kalanovic/Gross (Tuebingen), Ottensmeyer
  - open surgery
  - appl'ns: tissue characterization, surg. sim.
  - 20Hz bandwidth; 30° RoM; 0.45mNm torque
  - 6mm needle/adhesive tip; reference ring 16/20mm ID/OD
  - *in vivo* porcine liver, *in vitro* bovine liver





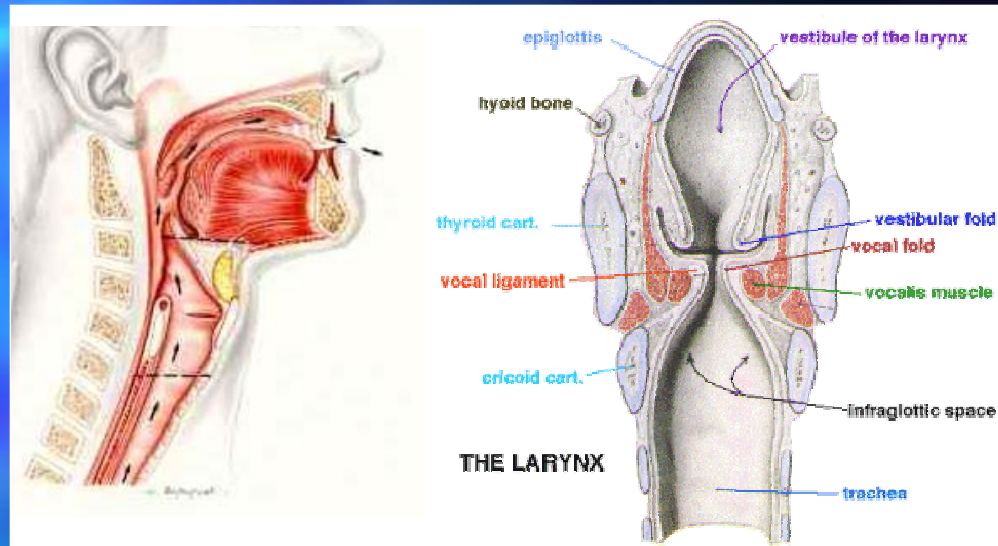
# Compliance: tangential shear

- The Larynx
  - airflow excites oscillation in vocal folds
  - stable, efficient sound production depends on geometry, visco-elasticity



# Compliance: tangential shear

- The Larynx
  - airflow excites oscillation in vocal folds
  - stable, efficient sound production depends on geometry, visco-elasticity
  
- Vocal fold damage
  - overuse
  - cancer
  - infectious disease



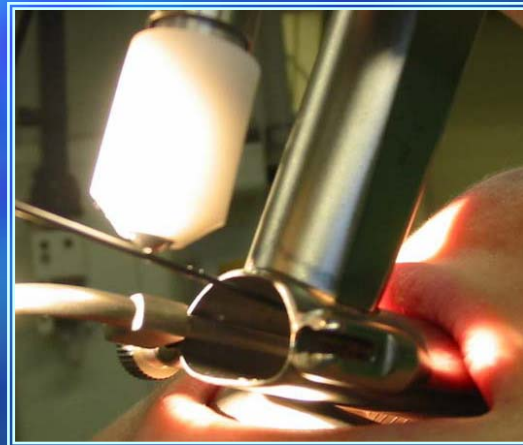
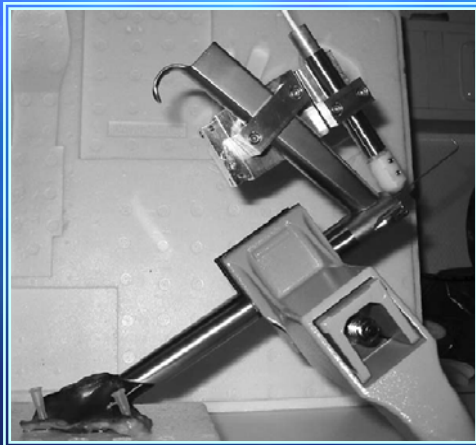
# Compliance: tangential shear

- Therapeutic concept:
  - Inject/implant biomaterial
    - synthetic gels
    - processed autologous fat
  - Necessary properties
    - long residence time; minimal inflammation, no rejection
    - *appropriate mechanical behavior!*
  - Two-part challenge
    - measure normal, healthy tissue response
    - measure implant behavior to confirm success



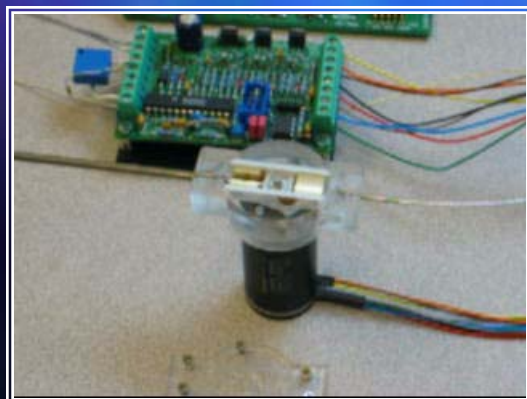
# Compliance: tangential shear

- DeMontfort U., Leicester, UK
  - Goodyer et al. 2006a,b:
    - human in vivo, quasi-static
    - fixed displacement step shear
    - pharmaceutical adhesive bonding
    - $G = 0.7\text{-}2.2$  kPa (possible over-estimate?)

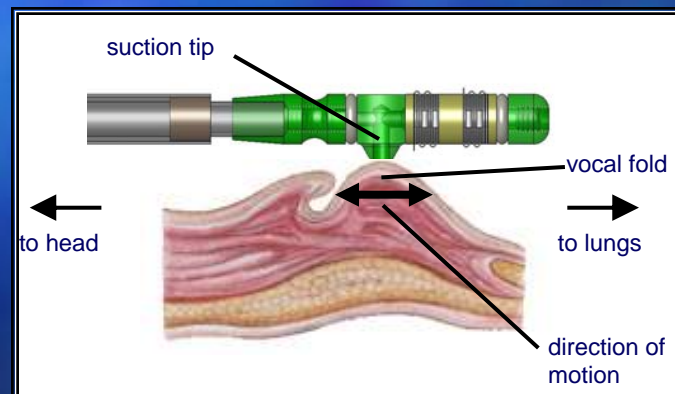


# Compliance: tangential shear

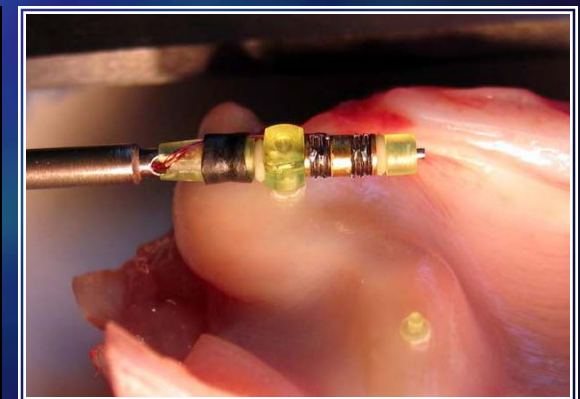
- Early tests with TeMPeST
  - unsuitable for intra-operative use
- Development of VoCCI
  - imposes tangential oscillation, records reaction force
  - Scotch yoke drive to  $>250\text{Hz}$ 
    - human vocal fundamental from 100-300Hz
    - 50% strain



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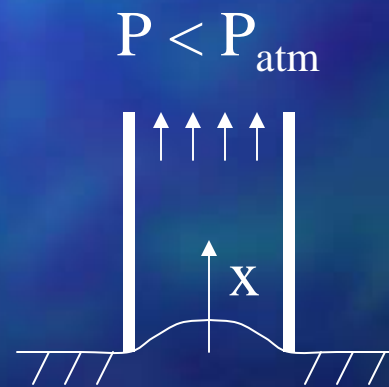
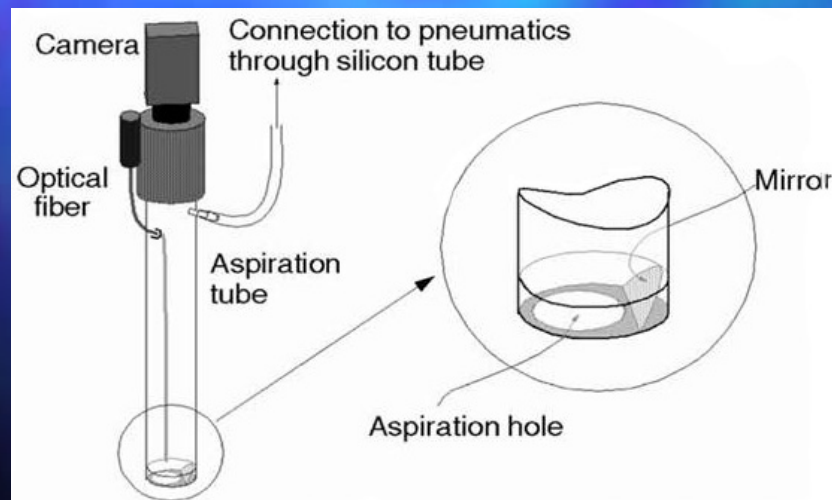
46



# Compliance: *last one!*

## Aspiration testing

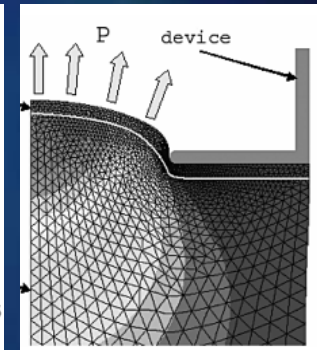
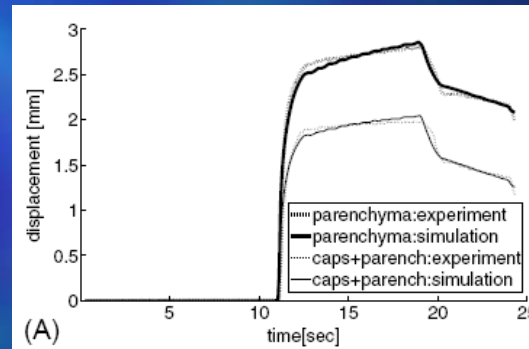
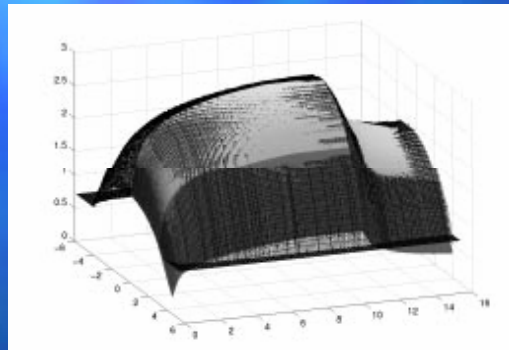
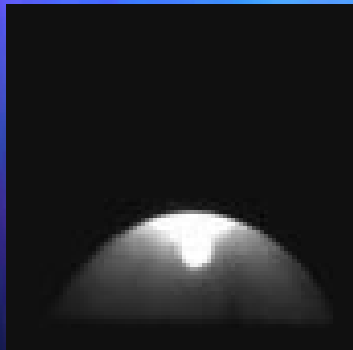
- ETH Zurich, Switzerland
  - Surgical simulation, prediction of cervical incompetence (loss of pregnancy)
  - human cervix in vivo, ex vivo; human liver
  - need for sterility
  - 30Hz frame rate; 3mm displacement observed; 100mbar vacuum; 12mm circular opening





# Compliance: aspiration testing

- Hollenstein et al., ISBMS'06
  - stronger pre-conditioning effect ex vivo
  - QLV model with capsule
  - parameter extraction using FEA

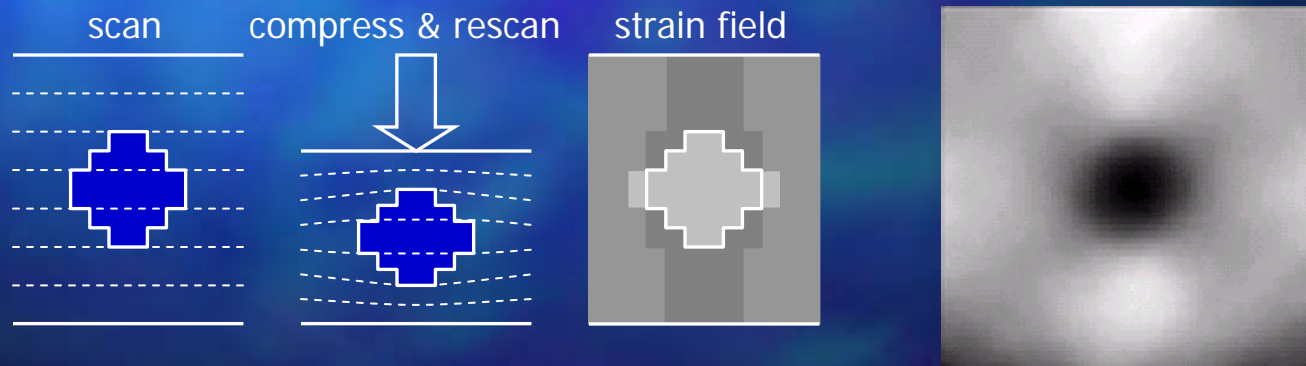


# Elastography

- Imaging techniques
  - Ultrasound
    - Real-time imaging (& inversion)
    - Mechanically deform tissue / focused US shear waves
    - 2-D imaging (with a few exceptions)
    - Estimate 3-D strain tensor
  - Magnetic Resonance Imaging
    - 3-D imaging, arbitrary directions w/equal sensitivity
    - Long scanning/computation times

# Elastography

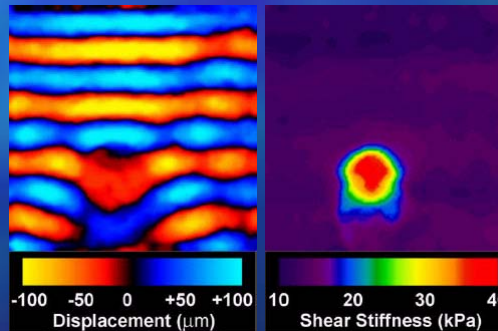
- Static deformation
  - Ultrasound: Ophir, et al., 1990
  - Magnetic Resonance Imaging: Plewes, et al. 1995
  - US: Scan pre- & post-deformation
  - Normalize, calculate strain & invert
  - Note strain artifacts





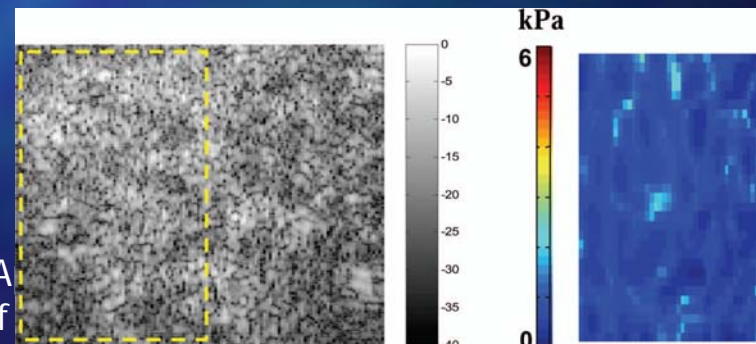
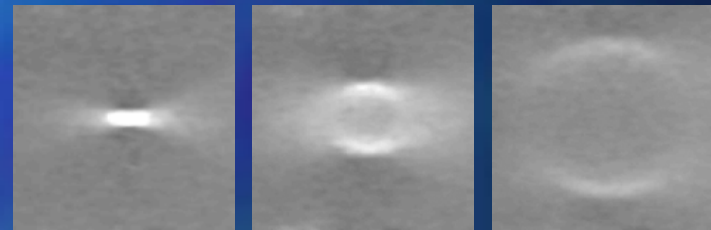
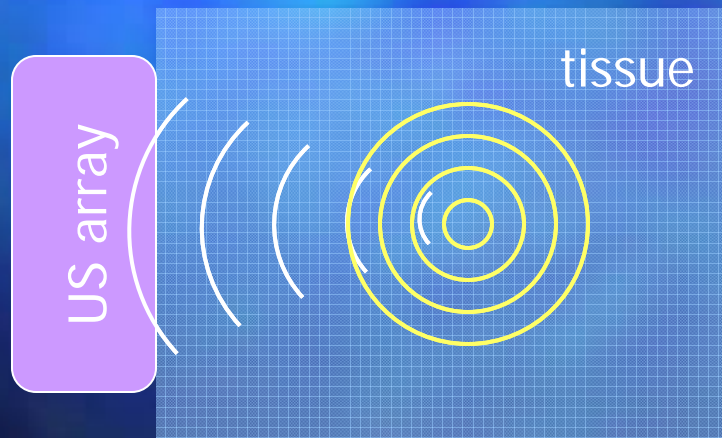
# Elastography

- Dynamic testing: mechanical stimulation
  - Lerner, et al., late '80s: "sonoelasticity imaging"
  - Muthupillai/Manduca/Ehman, ~'95: MRI
  - Mechanical surface vibration (normal or shear)
  - Measure local velocities/amplitude/shear wave velocity
  - Invert amplitude or direct calculation from shear wave velocity
    - $G = v_s^2 \rho$  for Hookean, isotropic medium



# Elastography

- Dynamic testing
  - Focused ultrasound as stimulus
    - Create local impulse (or train of impulses)
    - Observe traveling shear wave with high frame rate U/S
    - Elasticity related to shear wave velocity
    - Linear viscoelastic model: displacements  $\sim 10 \mu\text{m}$
    - Fink: Supersonic Shear Imaging: healthy human breast tissue, 1-3kPa Young's mod. (Bercoff et al., IEEE Ultrasonics Symp'03)



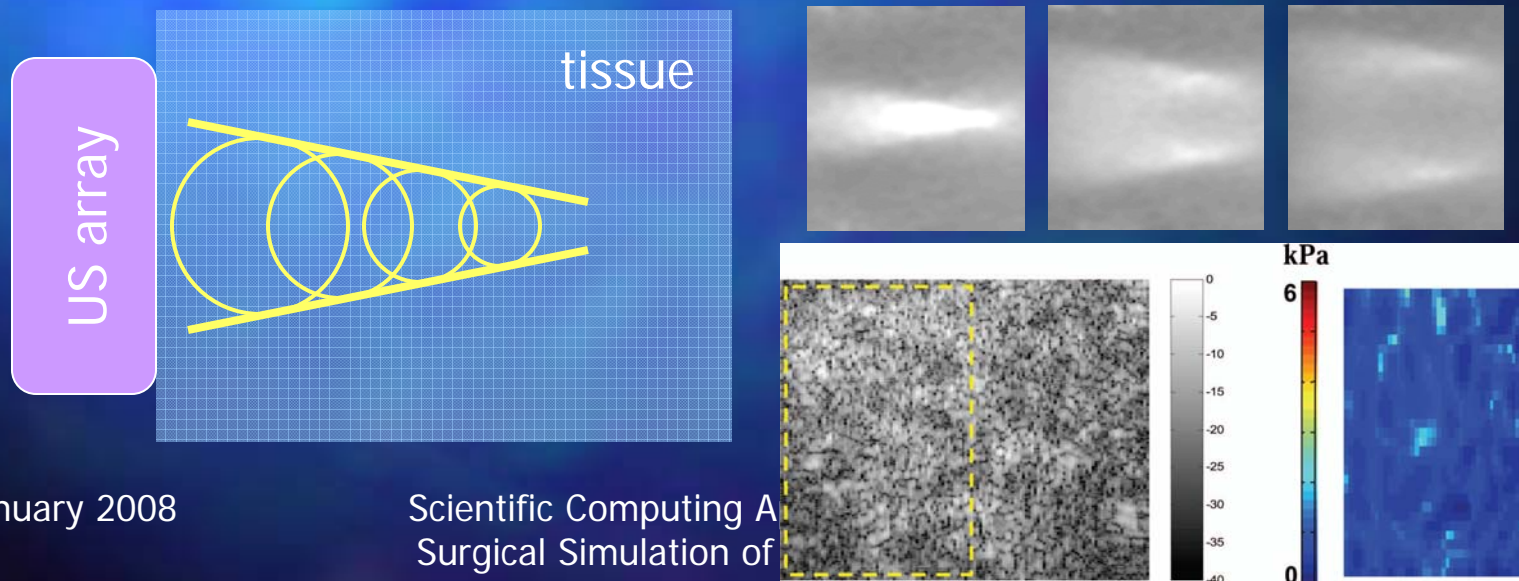
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Surgical Simulation of



# Elastography

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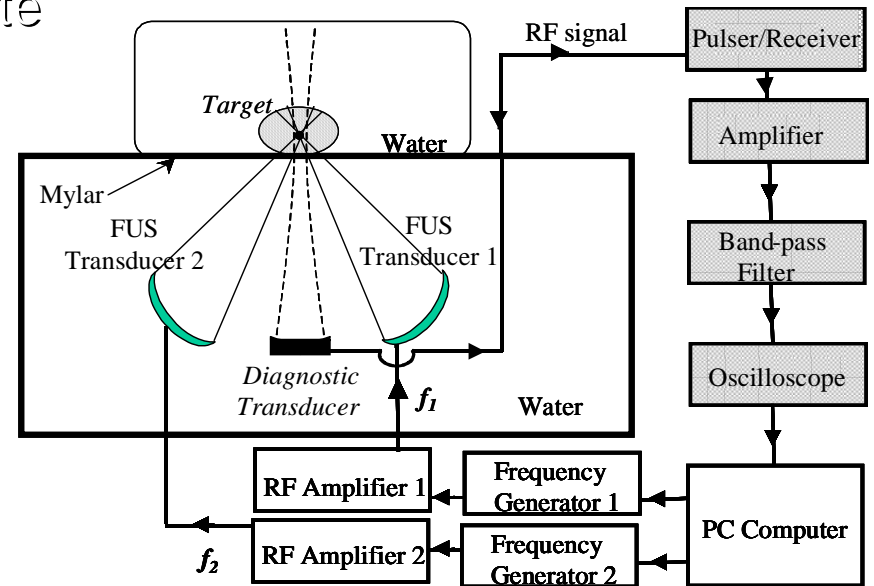
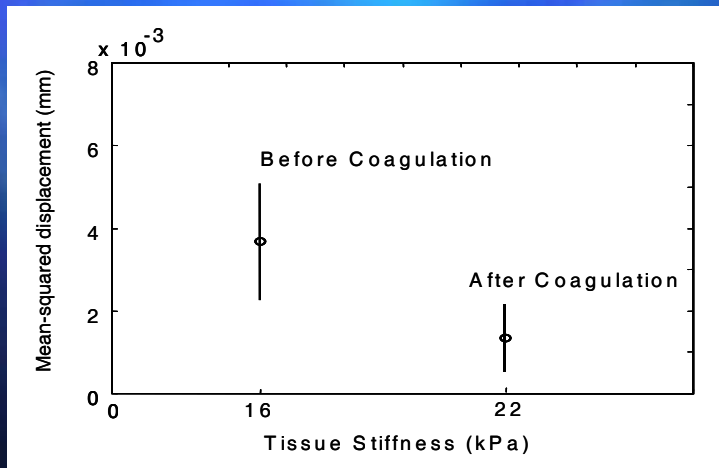
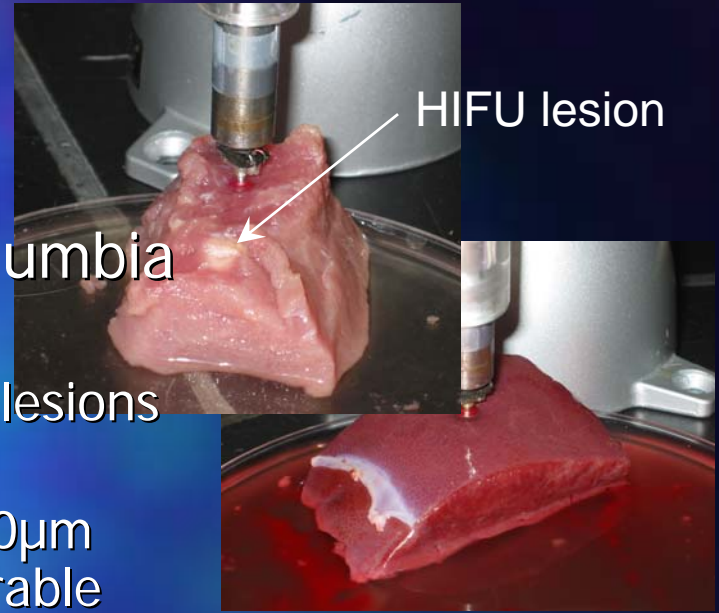
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Surgical Simulation of



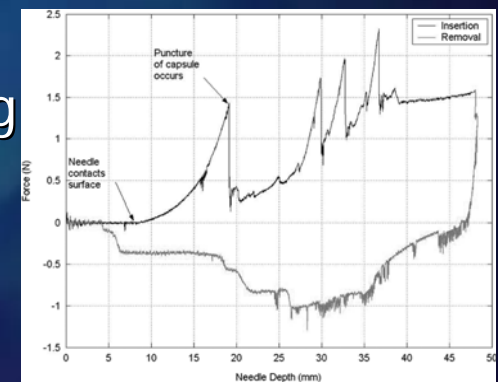
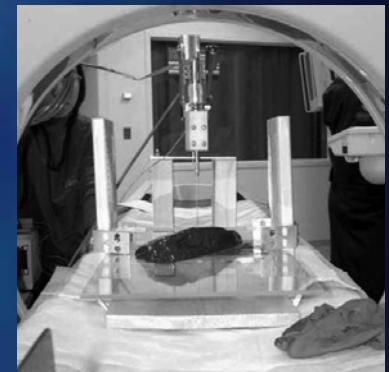
# Elastography

- HMI: Konofagou, et al.; BWH/Columbia
  - *in vitro* so far
  - appl'ns: creating and characterizing lesions in tissue (e.g. tumor ablation)
  - 200 & 800 Hz harmonic force; ~5-10 $\mu$ m amplitude; force not directly measurable
  - *in vitro* liver & muscle to date



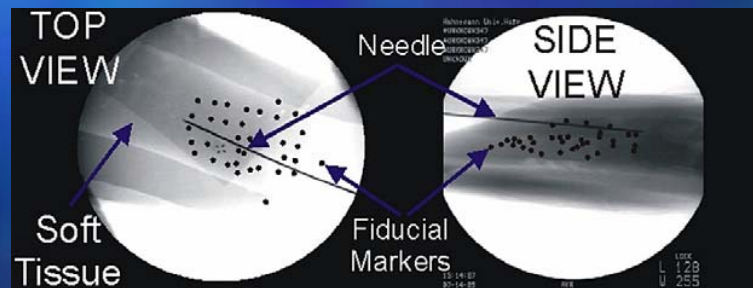
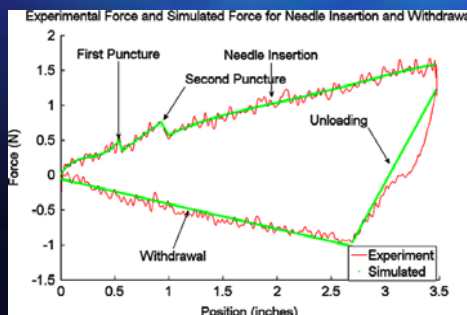
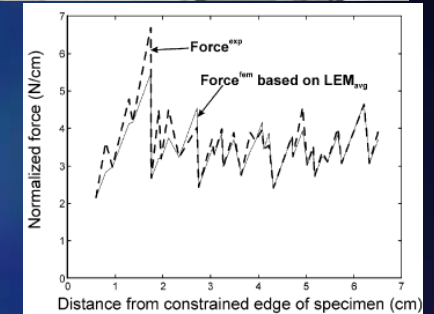
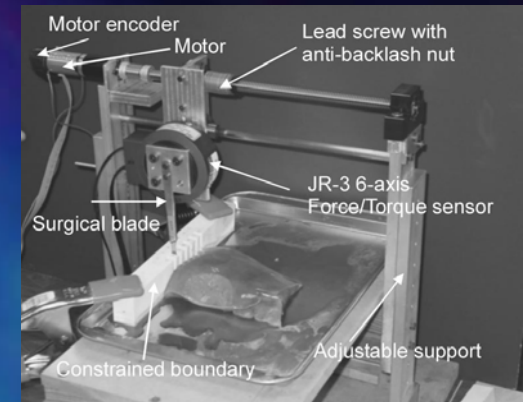
# Cutting & Needle Insertion

- More limited data, instruments
- Tendick (Brower et al., MMVR01)
  - measuring tool force on needle driver & scissors
  - 6-dof needle force, 1-dof cutting/spreading
  - 30Hz sampling
  - 3-0 suture through porcine stomach wall,
- Okamura, Haptics Exploration Lab, JHU
  - scissor cutting forces
    - IEEE Trans.Rob.'07, in press
  - percutaneous sim & needle insertion modeling
    - Elastic response, puncture, Karnopp friction
    - Okamura et al., IEEE TBME'04

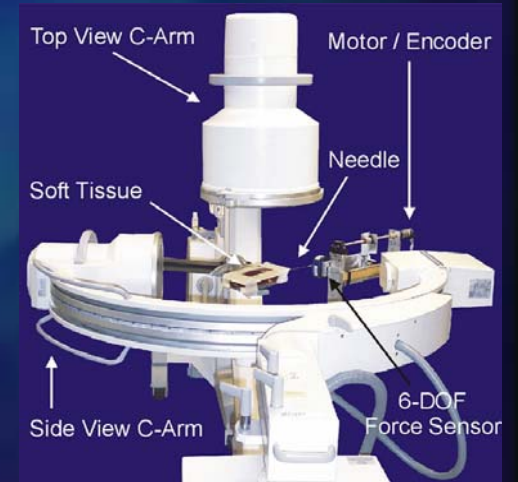


# Cutting & Needle Insertion

- Desai, RAMS Lab, U.Maryland
  - single blade cutting
    - varying cutting speed, blade angle
    - developed model predicting elastic slope, fracture model
    - Chanthasopeehpan et al., TBME'07a,b
  - needle insertion
    - fluoro imaging of tissue, needle, internal fiducials
    - position/force tracking, porcine tissue in vitro
    - generated simulation w/haptics of needle insertion



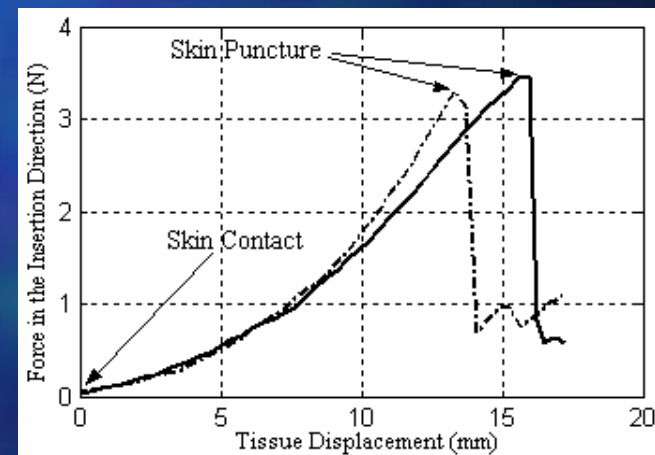
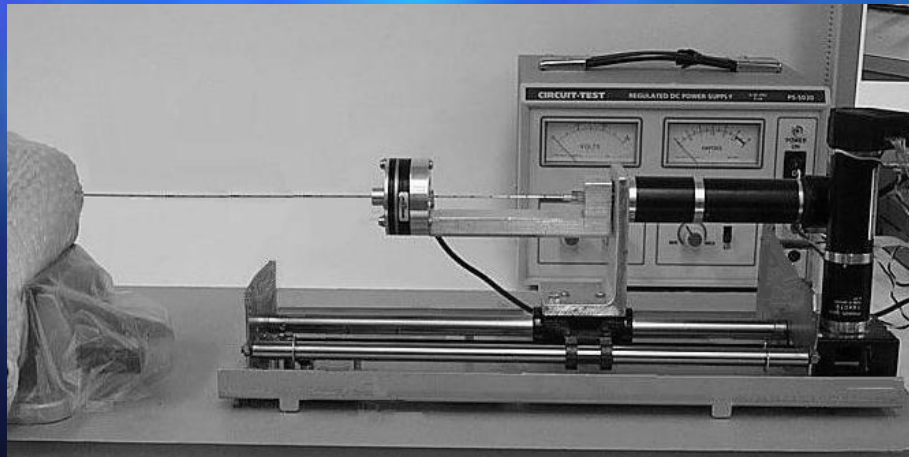
Scientific Computing Applications in Surgical Simulation of Soft Tissues





# Cutting & Needle Insertion

- U. Western Ontario, Canada
  - Abolhassani, ProcEMBS'04
  - bevelled needle insertion for prostate brachytherapy
  - axial/rotational instrument, 6-DoF force sensing
  - turkey tissue model, insertion rate testing
  - Excellent survey paper: Abolhassani et al., MedEng&Phys'07



# Summary

- Wide range of techniques
  - compliance testing
    - compression, tension, indentation, torsion, aspiration
    - quasi-static to 100Hz—full range of surgical strain rates
    - extremely small to large deformations
  - elastography, coming up, some clinical uses
    - small deformations have questionable application to surg. sim.
    - current applications for diagnostic purposes
  - topology-altering testing
    - needle insertion, scalpel, scissors
    - limited available data
- growing body of *in vivo* data, including *human*
  - still need more organs, improved constitutive models (& parameters), healthy vs. other conditions...

# And a few other notes...

**AIMS**

*Educating America about the Value of Medical Simulation*

*Advanced Initiatives in Medical Simulation*

- **AIMS: Advanced Initiatives in Medical Simulation**
  - 501(c)(6) non-profit consortium (“lobby group”)
  - promotes medical simulation for improving patient safety, reducing errors, ensuring competency, reducing costs...
  - improve awareness, unify the “message”, secure resources
  - **Enhancing SIMULATION Act, 2007 (H.R.4321)**
    - (Safety In Medicine Utilizing Leading Advanced Simulation Technologies to Improve Outcomes Now)
    - reps Forbes (R-VA), Kennedy (D-RI)
- **SAVE THE DATE: 5<sup>th</sup> Annual AIMS Conference & Exhibition**
  - May 6-7, 2008, Washington, DC
  - attended by industry, academia, members of congress
- [www.medsim.org](http://www.medsim.org)



# And a few other notes...

**AIMS**

*Educating America about the Value of Medical Simulation*

*Advanced Initiatives in Medical Simulation*

## ■ **AIMS: Advanced Initiatives in Medical Simulation**

HR4321 calls for:

- federal funding for Centers of Excellence for med sim R&D
- support for solving challenges in med sim
- grants for academic sites to acquire simulators
- support to develop curricula integrating simulation
- grants to accreditation organizations for standards development
- federal med sim coordinating council
- \$50,000,000 for FY'08, sums as necessary for FY'09-'12

## ■ **SAVE THE DATE: 5<sup>th</sup> Annual AIMS Conference & Exhibition**

- May 6-7, 2008, Washington, DC
- attended by industry, academia, members of congress

## ■ [www.medsim.org](http://www.medsim.org)

# And a few other notes...

- **ISBMS'08: International Symposium on Computational Models for Biomedical Simulation**
  - July 7-8, 2008. London, UK
  - [www.imperial.ac.uk/medicine/isbms08](http://www.imperial.ac.uk/medicine/isbms08)
  - Topics of Interest:
    - anatomical modeling; hard & soft biomechanics; physiological models; validation; simulators; haptics; GPU-based sim; etc.
  - 12 March 2008: full papers due (8 page max)
  - successor to IS<sup>4</sup>TM'03 (INRIA), ISMS'04 (CIMIT), ISBMS'06 (ETH)



# And a few other notes...



- IMSH'08: International Meeting on Simulation in Healthcare
  - January 13-16, 2008. San Diego, CA
  - [www.ssih.org](http://www.ssih.org)
  - Users, developers, stakeholders in mannequin & computer-based simulators, VR systems, standardized patients, task trainers
  - This year: 1<sup>st</sup> Technology Track workshop series
    - physical sim development; software-based sim (Harders); cross-platform issues (tissue props, realism, etc.); contact between end users and academic/industrial developers



# Questions & further information

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[www.medicalsim.org](http://www.medicalsim.org)

[www.cimit.org](http://www.cimit.org)

[ottensmeyer.mark@mgh.harvard.edu](mailto:ottensmeyer.mark@mgh.harvard.edu)

- Support for some of this work provided by the Department of the Army, grant number DAMD 17-01-1-0667 and by the Institute of Laryngology and Voice Restoration. The ideas and opinions expressed to not necessarily represent those agencies.