

Multiscale analysis of fMRI data

François G. Meyer
Department of Electrical Engineering
University of Colorado at Boulder

`francois.meyer@colorado.edu`
`http://ece-www.colorado.edu/~fmeyer`

Collaborators

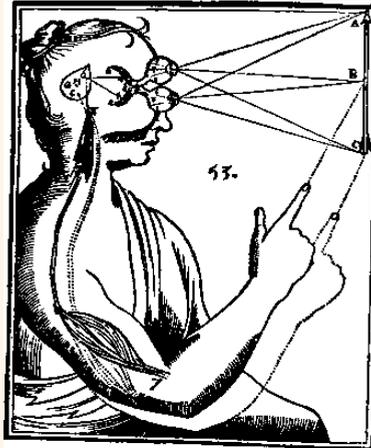
- Xilin Shen
- Jatuporn Chinrungrueng

Outline

1. Introduction
2. FMRI projections on wavelet packets
3. Statistical properties of the projections
4. Detection of activation
5. Experiments

Introduction

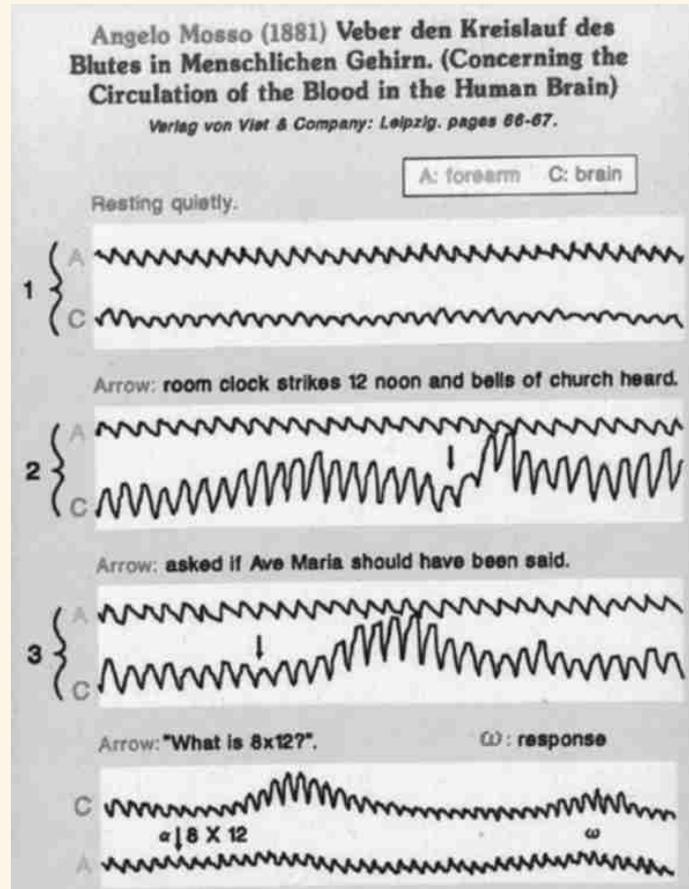
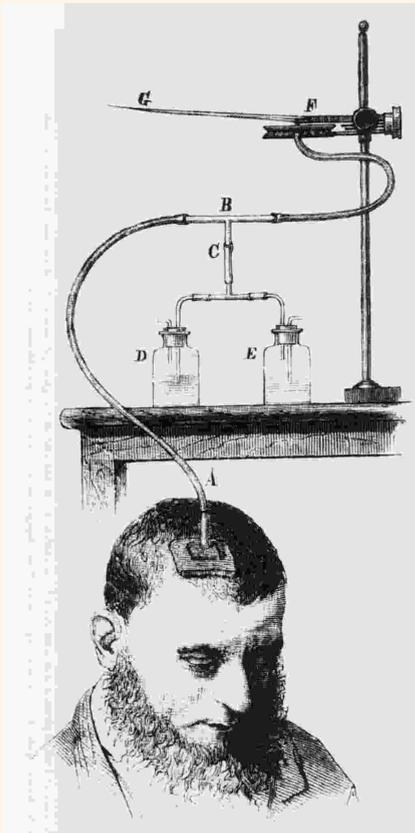
- functional imaging : delineation of functional anatomy in terms of spatial and temporal organization



René Descartes *De homine* (1662)

Functional brain imaging : blood flow

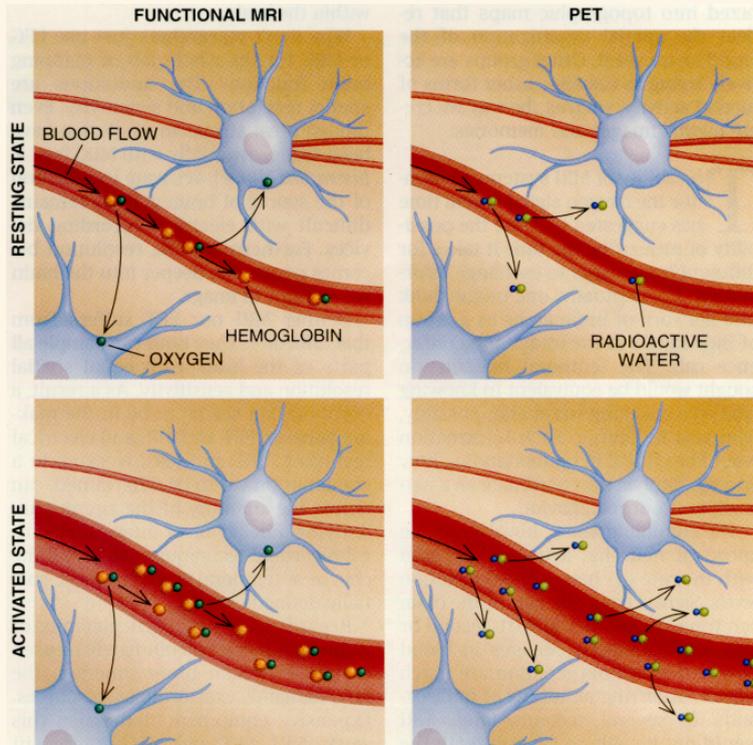
- hemodynamic changes induced by neuronal activity when a subject is submitted to sensory or cognitive stimulations.



Detection devices



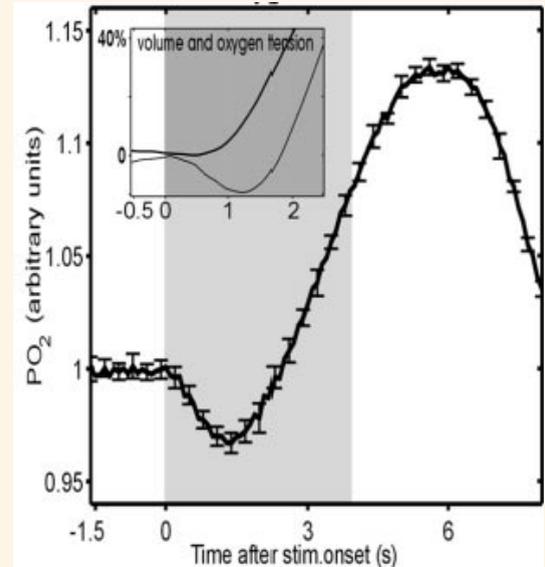
PET/fMRI



PET, fMRI : neuronal activity requires energy. Local increases in blood flow, and metabolism can be measured.

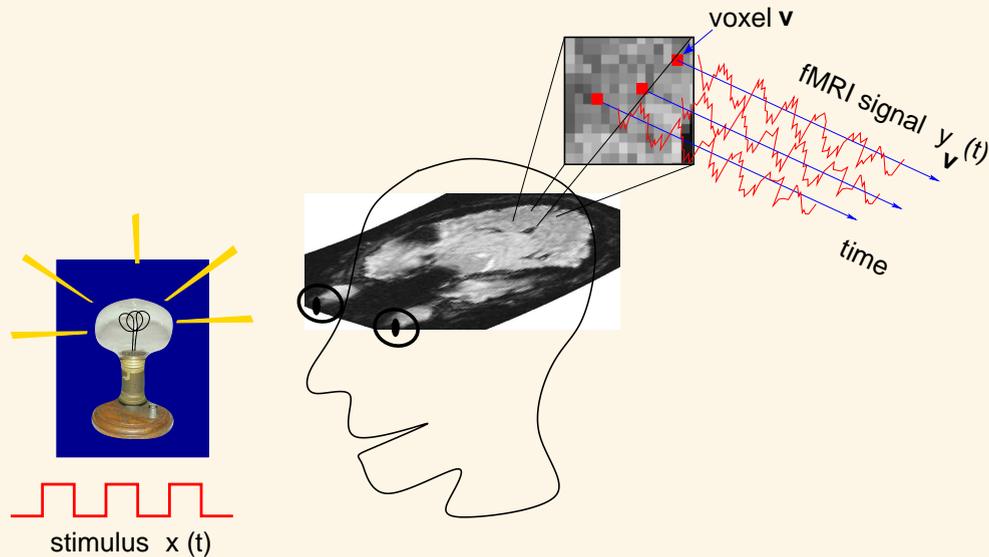
Oxygen concentration changes in the microcirculation

- Initial increase in oxygen consumption created by metabolic demand
- Increase in cerebral blood flow : oversupply of oxygenated blood
- oxygenated hemoglobin induces a difference in magnetic susceptibility relative to the surrounding
- imbalance between oxygen metabolism and oxygen supply is at the origin of the BOLD contrast



Microvascular oxygen concentration
[Vanzetta and Grinvald, 1999].

Functional Magnetic Resonance Imaging (fMRI)



- Goal of the analysis : detect “activated” voxels v where changes in the fMRI signal y are triggered by the stimulus x .

Analysis of fMRI data : Univariate statistical models

1. General Linear Model [Friston et al., 1995]

$$\mathbf{y}_v = \mathbf{X}\boldsymbol{\beta} + \boldsymbol{\varepsilon}, \quad \boldsymbol{\varepsilon} \sim \mathcal{N}(0, \boldsymbol{\Sigma}) \quad (1)$$

limitations :

- $\boldsymbol{\varepsilon}(t)$ correlated
- $\text{var}(\boldsymbol{\varepsilon})$ varies as a function of \mathbf{v} [Chen et al., 2003]

2. Linear Time Invariant Model

$$\mathbf{y}_v = h_v * \mathbf{x} \quad (2)$$

[Lange and Zeger, 1997, Genovese, 2000]

limitations :

- h_v haemodynamic response function depends on brain region, subject, etc.
- nonlinear relationship between \mathbf{y}_v and \mathbf{x} [Friston et al., 1998, Miller et al., 2001, Rees et al., 1997, Vazquez and Noll, 1998].

Analysis of fMRI data : Exploratory methods

1. principal component analysis

[Lai and Fang, 1999, Gabbay et al., 2000]

limitations :

- components need to be orthogonal
- interpretation of the components ?

2. independent component analysis

[B.B.Biswal and Ulmer, 1999, McKeown, 2000]

limitations :

- component maps need to be independent
- interpretation of the components ?

3. Clustering of the time series \mathbf{y}_v

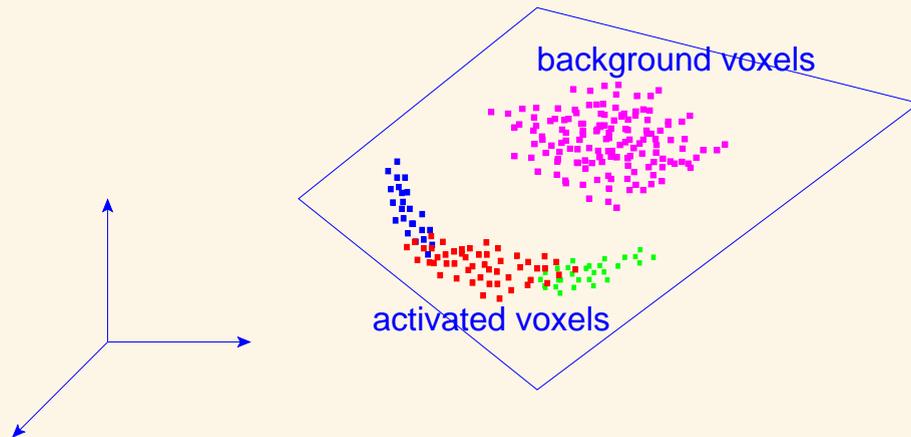
[Baumgartner et al., 1998, Golay et al., 1998, Meyer and Chinrungrueng, 2000]

limitations :

- performed in the time domain (\mathbb{R}^{128} !)

Goal of this work

- search for projections of the fMRI time series on a low dimensional subspace :
→ reveal the presence of activated time series.



- probability distribution of the projections (coefficients) :
finite mixture of multivariate Gaussian densities
- estimate the parameters of the mixture, number of components, and interpret their physiological roles.

What type of projections ?

properties of the fMRI time series :

- non stationary → analyze transients, local features
- long range dependence ($1/f$ spectral behavior)
[Zarahn et al., 1997, Fadili and Bullmore, 2002]
→ whiten the time series, stationary

good properties of the projections :

- rich library of waveforms well localized in time and in frequency
- fast search in the library

→ library of wavelet packets

What can we learn from the wavelet packet coefficients of fMRI time series ?

- background signal: $y_{\mathbf{v}}(t) = \text{constant} \rightarrow \alpha_{\mathbf{v}} \simeq 0$
 $\alpha_{\mathbf{v}} \sim \mathcal{N}(0, \sigma_b^2)$ [Chen et al., 2003]
- activated signal: $y_{\mathbf{v}}(t) = \text{response triggered by stimulus}$
if ψ is well chosen then $\alpha_{\mathbf{v}} \sim \mathcal{N}(\mu_k, \sigma_k^2)$ [Meyer and Shen, 2004]
- strength μ_k may vary as a function of \mathbf{v}
- $\alpha_{\mathbf{v}}$ stationary, uncorrelated

$$\text{corr}(\alpha(j, k), \alpha(j', k')) \sim O(|2^{-jk} - 2^{-j'k'}|^{\gamma-2p-1}),$$

p vanishing moments

Joint distribution of the wavelet packet coefficients

- choose a small number K of wavelet packets ψ_{γ_k} , (e.g. $K = 3$)
- for \mathbf{v} all over the brain, compute $\alpha_{\mathbf{v}}(\gamma_k)$
- joint distribution of vector of coefficients $\boldsymbol{\alpha} = [\alpha(\gamma_0), \dots, \alpha(\gamma_{K-1})]^T$
- $\boldsymbol{\alpha} \sim$ finite mixture of M multivariate Gaussian densities

$$p(\boldsymbol{\alpha}) = \sum_{m=1}^M \pi_m \boldsymbol{\phi}(\boldsymbol{\alpha}, \mu_m, \Sigma_m). \quad (3)$$

$\boldsymbol{\phi}$: K -multivariate normal density,

π_m : mixing parameters $\pi_m \geq 0$, $\sum \pi_m = 1$

- voxels with a similar activation strength are grouped together in the same component (irrespective of their relative spatial proximity).

Estimation of the parameters of the mixture

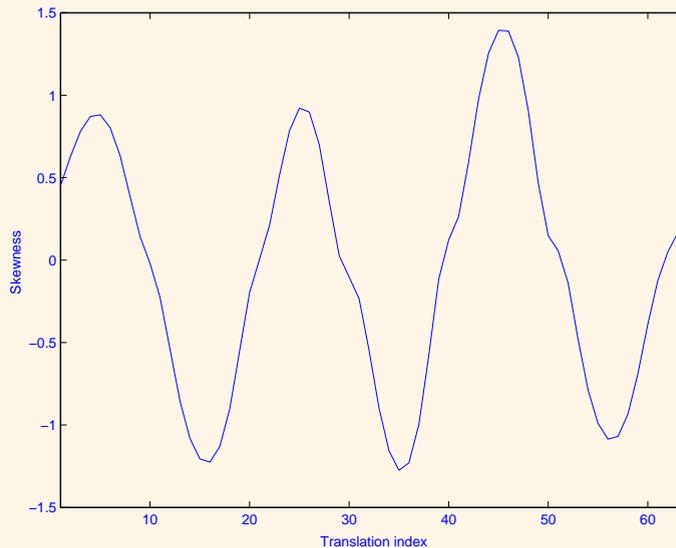
- maximum likelihood estimates $\hat{\mu}_m$, $\hat{\Sigma}_m$ and $\hat{\pi}_m$
- Expectation Minimization (EM) algorithm

How to find good a projection ?

- projection = ψ_γ nondecimated wavelet packet
- ψ_γ is a good projection if the distribution of the coefficients $\alpha_v(\gamma)$ is asymmetric:
 - many small coefficients (=background),
 - few large coefficients (=activated region)
- maximize the skewness of the distribution of $\alpha_v(\gamma)$ computed over all v

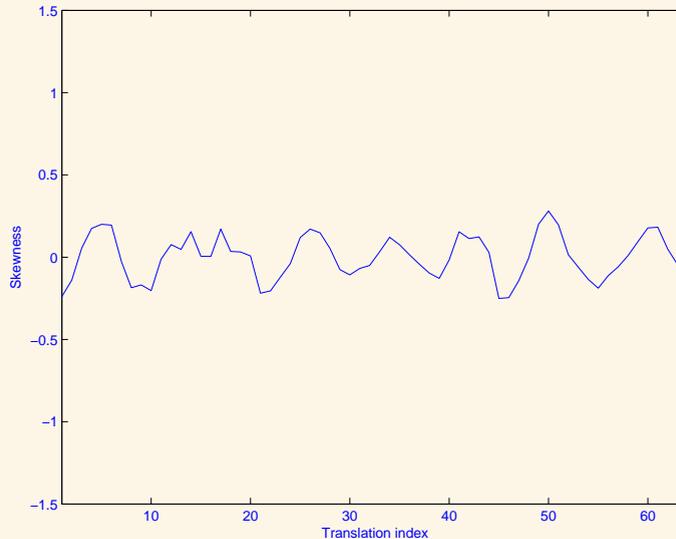
$$E[(X - EX)^3] / E[(X - EX)^2]^{3/2} \quad (4)$$

Skewness as a function of the translation index for a good projection



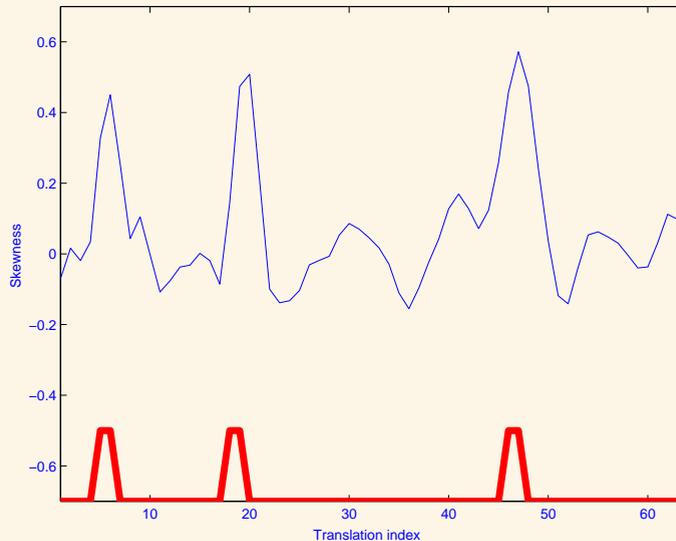
- periodic stimulus
- if ψ_γ is properly aligned:
 - response = large $\alpha_v(\gamma)$, background = small $\alpha_v(\gamma)$
 - asymmetric distribution
- misalignment:
 - response = small $\alpha_v(\gamma)$, background = small $\alpha_v(\gamma)$

Skewness as a function of the translation index for a bad projection



- for all translation indexes:
response = small $\alpha_v(\gamma)$, background = small $\alpha_v(\gamma)$
→ symmetric distribution

Skewness as a function of the translation index for a good projection



- 3 random stimuli
- for the right translation indexes:
response = large $\alpha_v(\gamma)$, background = small $\alpha_v(\gamma)$

A spatial prior

- spatial distribution of the pattern of activation :
not present in the mixture model
- activated patterns = small numbers of compact regions
- prior probability of the patterns of activation
- Markov random field
- detection of activation :

$$a_i = \begin{cases} 1 & \text{if } \mathbf{v}_i \text{ is activated,} \\ 0 & \text{if } \mathbf{v}_i \text{ is a background voxel.} \end{cases} \quad (5)$$

Parameter Estimation

- most likely activation pattern $\hat{\mathbf{a}}$:

$$\hat{\mathbf{a}} = \underset{(a_0, \dots, a_4)}{\operatorname{argmax}} p(\mathbf{a}|\boldsymbol{\alpha}) \quad (6)$$

- Bayes' theorem

$$p(\mathbf{a}|\boldsymbol{\alpha}) \propto p(\boldsymbol{\alpha}|\mathbf{a})p(\mathbf{a}) \quad (7)$$

- coefficients conditionally independent given the activation map

$$p(\boldsymbol{\alpha}|\mathbf{a}) = \prod_j p(\boldsymbol{\alpha}_{\mathbf{v}_j}|\mathbf{a}) = \prod_j p(\boldsymbol{\alpha}_{\mathbf{v}_j}|a_j) \quad (8)$$

- $p(\boldsymbol{\alpha}_{\mathbf{v}_j}|a_j)$ computed at each voxel \mathbf{v}_j from the mixture model
- $p(\mathbf{a})$: spatial prior
- optimization: simulated annealing

Experiments : synthetic data blended with in-vivo fMRI noise

- haemodynamic response [Glover, 1999] :

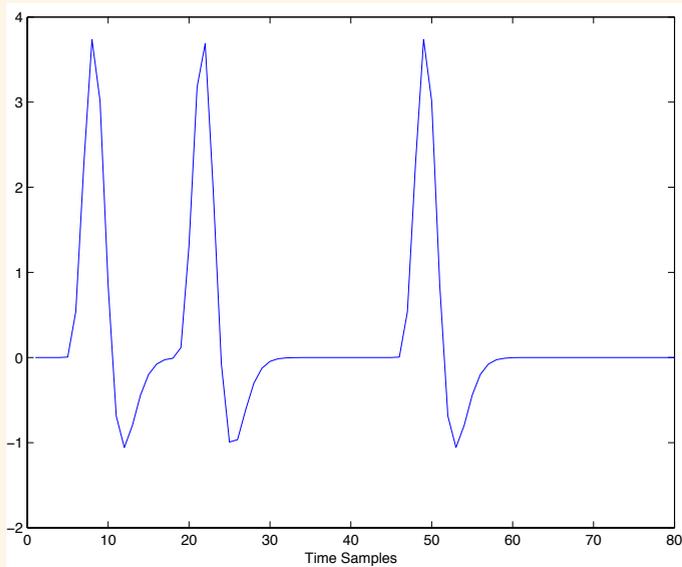
$$h(t) = A \left\{ a_1(t - t_s)^5 e^{-(t-t_s)/t_1} - 0.4 a_2(t - t_s)^2 e^{-(t-t_s)/t_2} \right\} \quad (9)$$

- A = strength of the response
- fMRI signal = $h * \text{stimulus} + \text{noise}$
- stimulus = 3 random events
- noise extracted from *in vivo* background time series

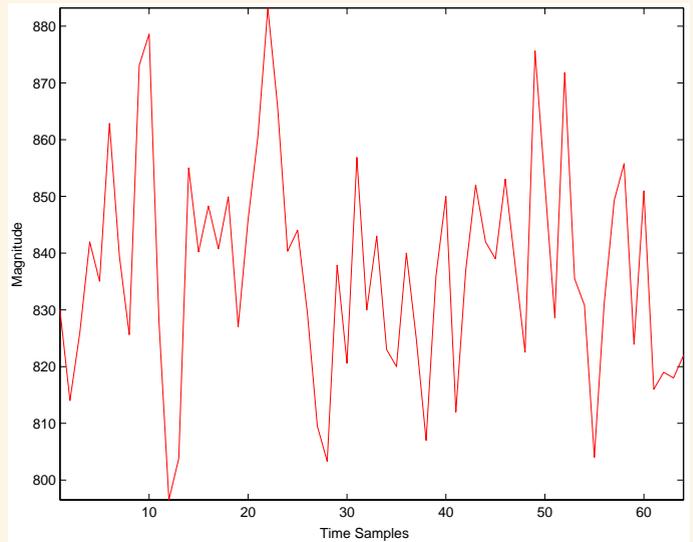
The synthetic datasets

- 4 datasets with uniform strength: $A = 1, 1.5, 2, 2.5,$
- 1 dataset with different strengths: A varies with v
- 108 activated voxels (6.75%)
- gold standard: linear regression with perfect knowledge of $h(t)$ and the stimulus

Time series

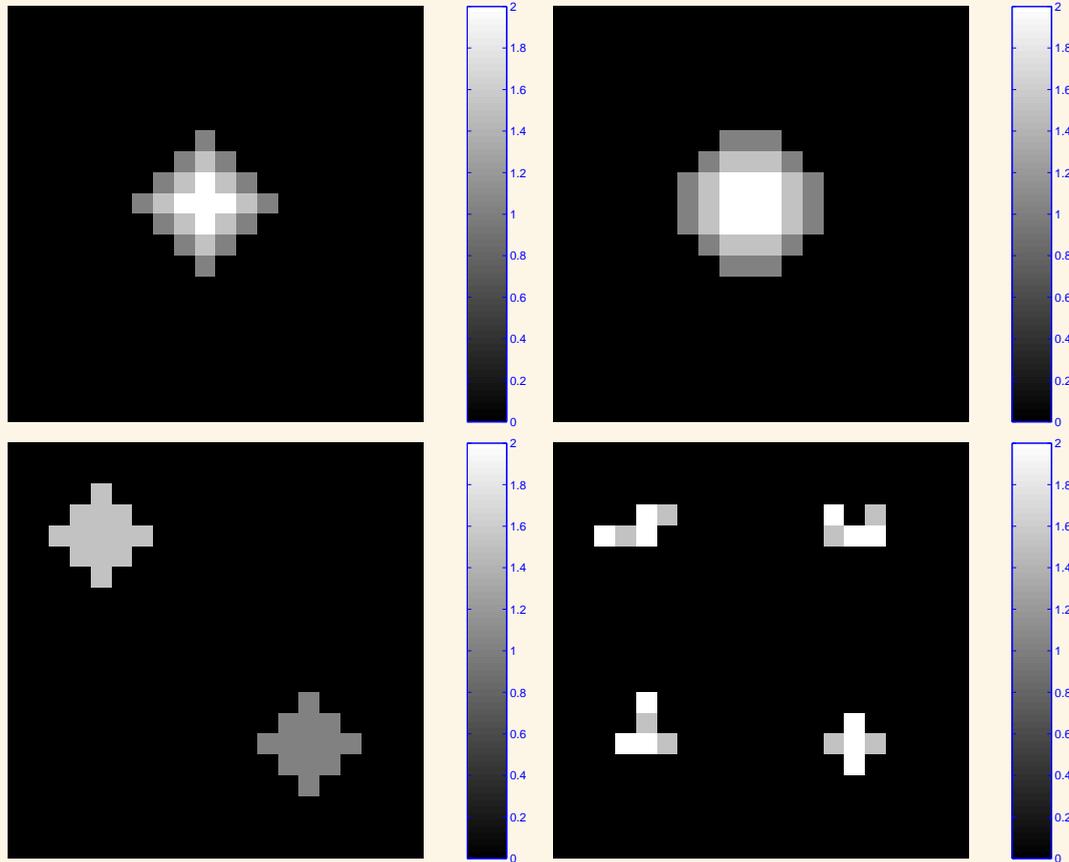


$h * \text{stimulus}$

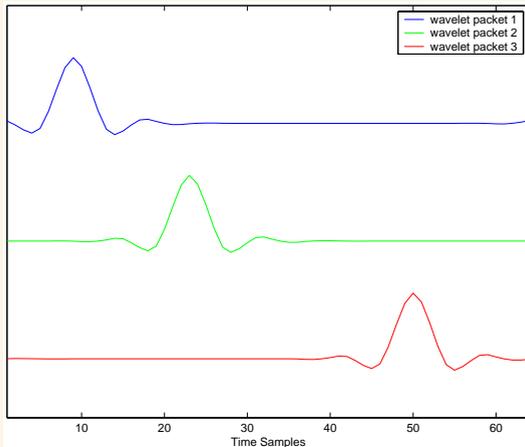


$h * \text{stimulus} + \text{noise}, A = 1$

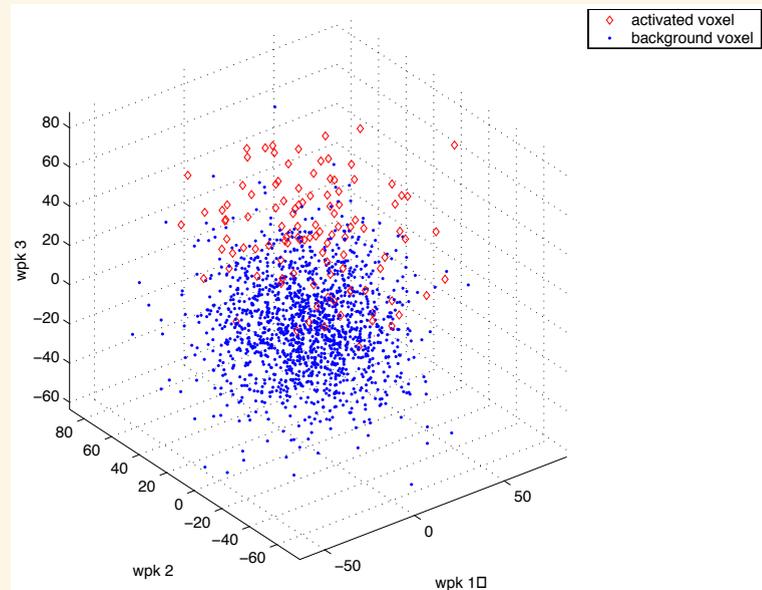
Dataset 5: activation patterns



Synthetic datasets: results

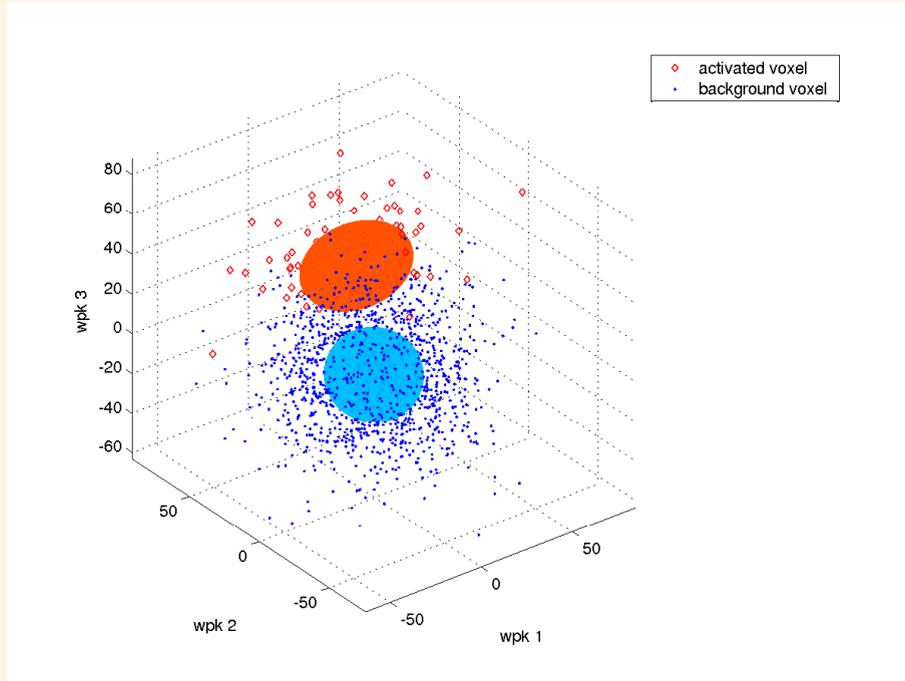


Projections ($K=3$)



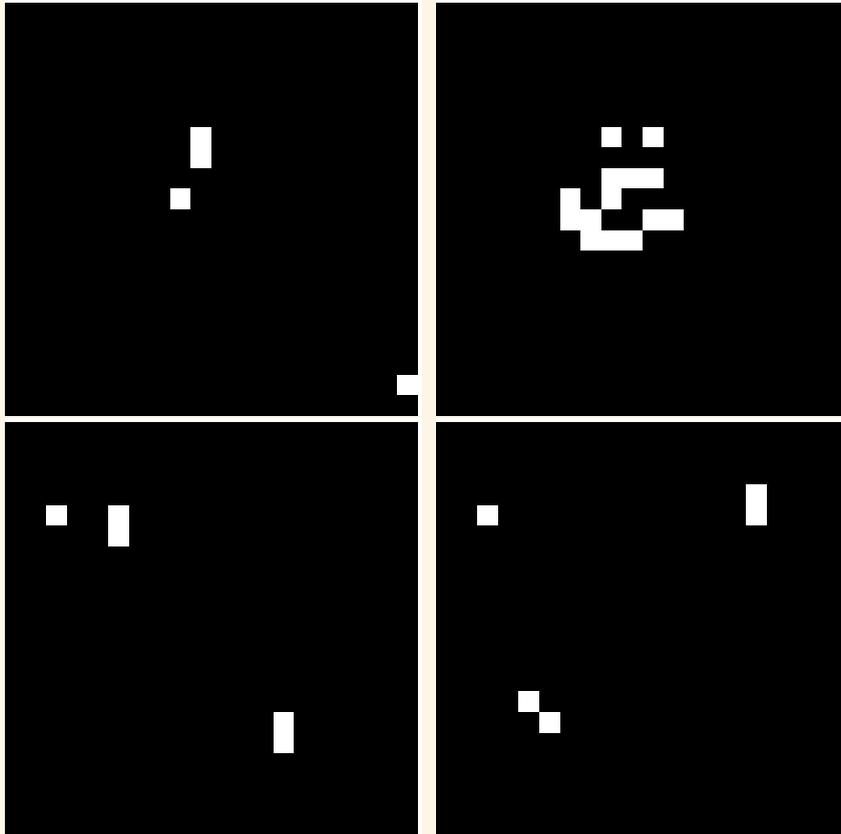
background (blue) and
activated (red) time series ($A = 1$)

Synthetic datasets: results



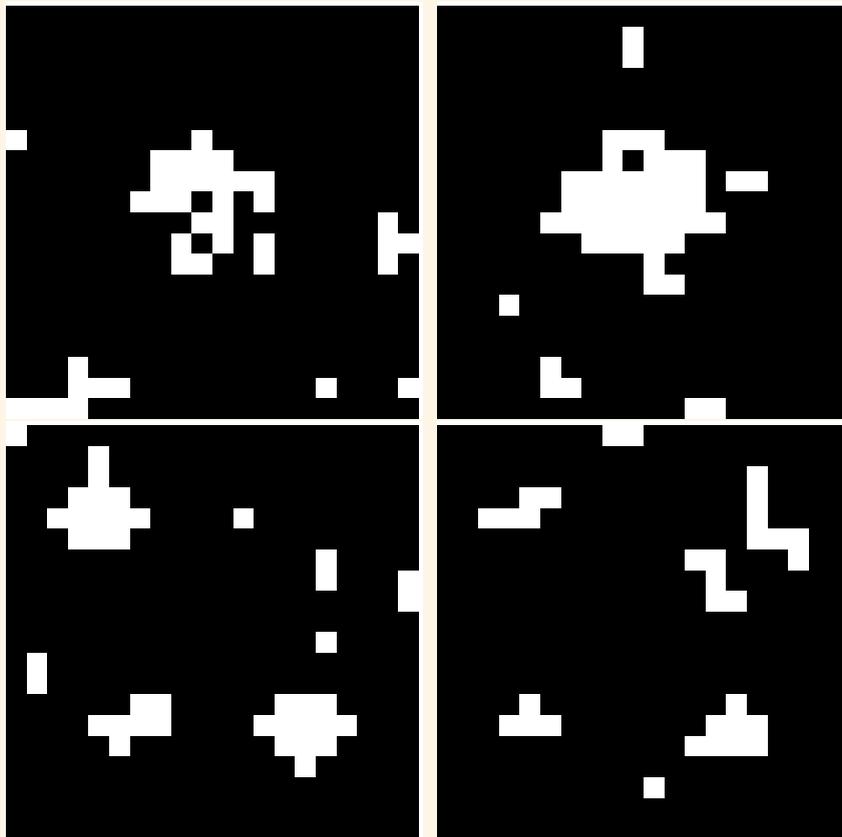
Classification between activated and background voxels ($A = 1$)

Synthetic datasets: activation maps



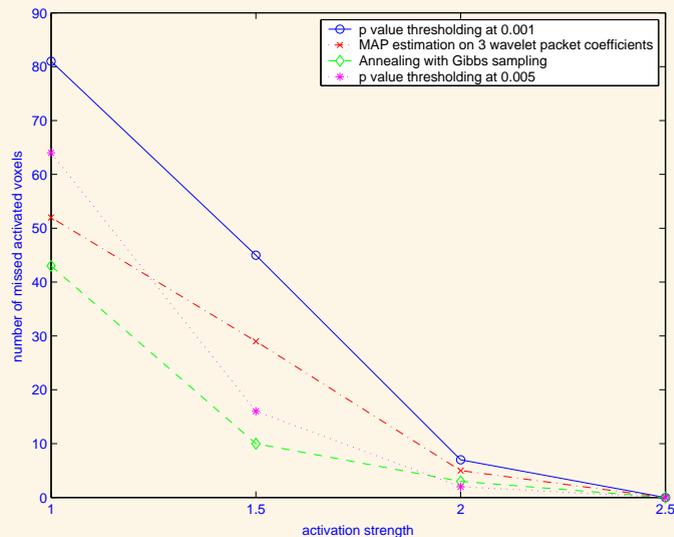
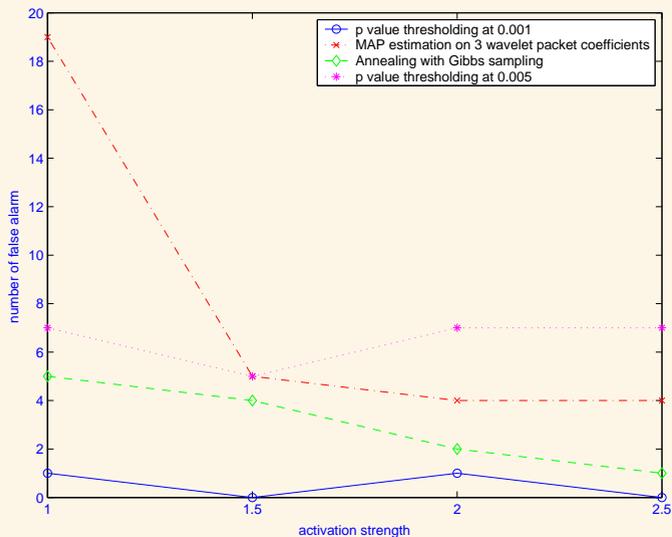
Activation maps obtained with the linear regression

Synthetic datasets: activation maps



Activation maps with our method ($A = 1$)

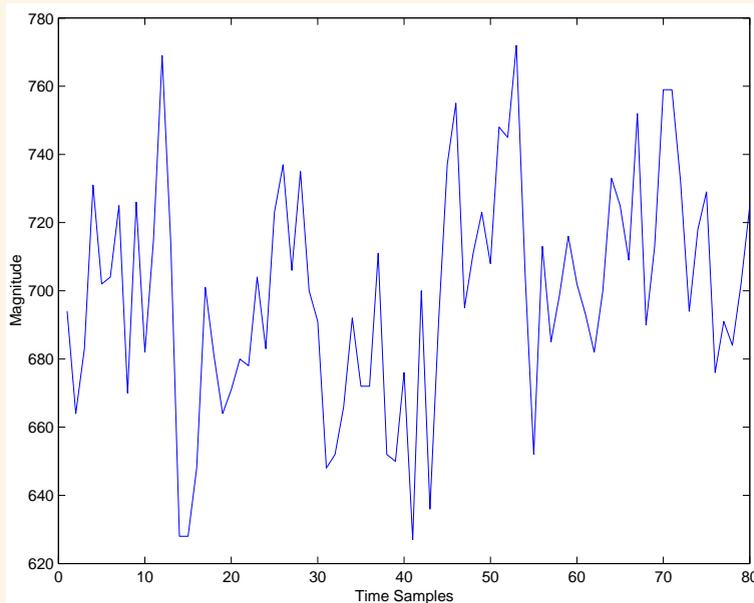
Performance



False alarm and missed activated voxels as a function of A .

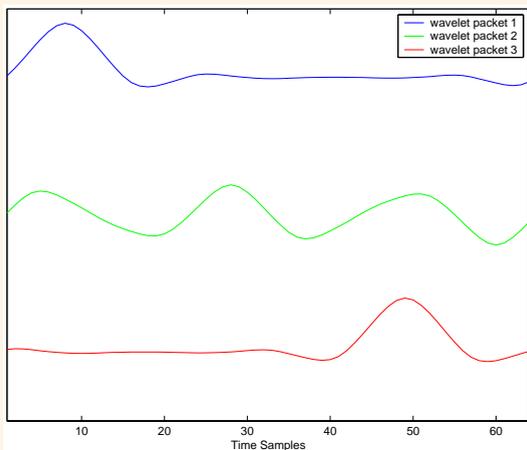
Experiments : in vivo data

- visual stimulus : periodic flashing checkerboard

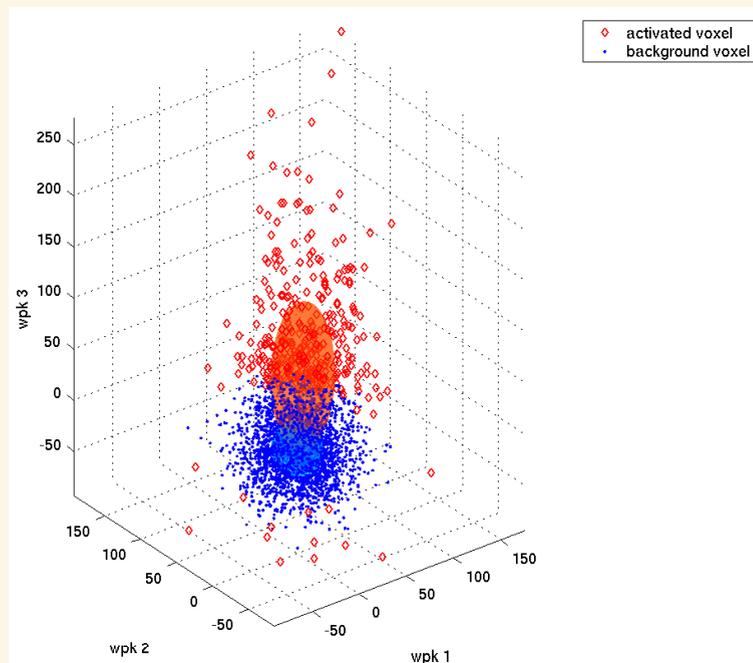


Time series from an activated voxel

Experiments : in vivo data

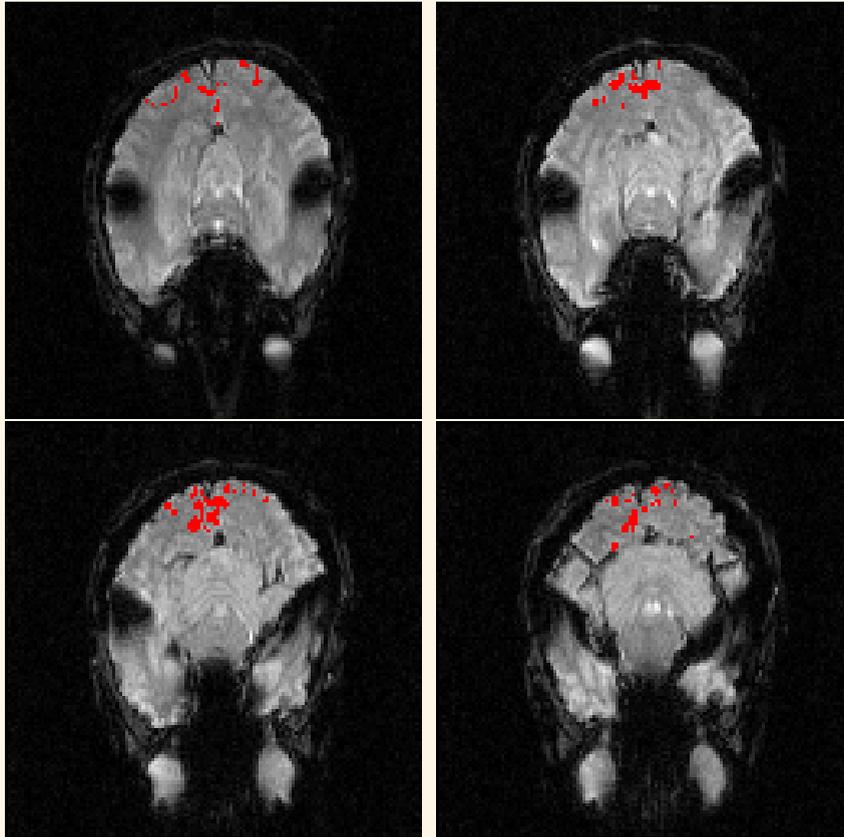


Projections (K=3)



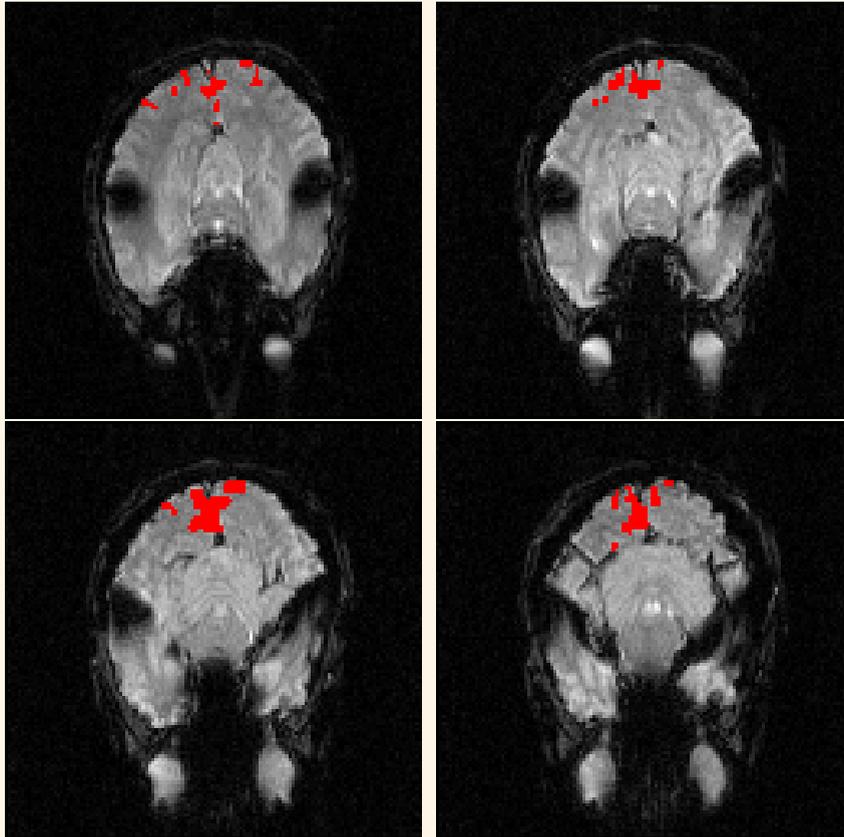
background (blue) and activated (red) time series

Visual stimulus: activation maps



Activation maps obtained with a linear model

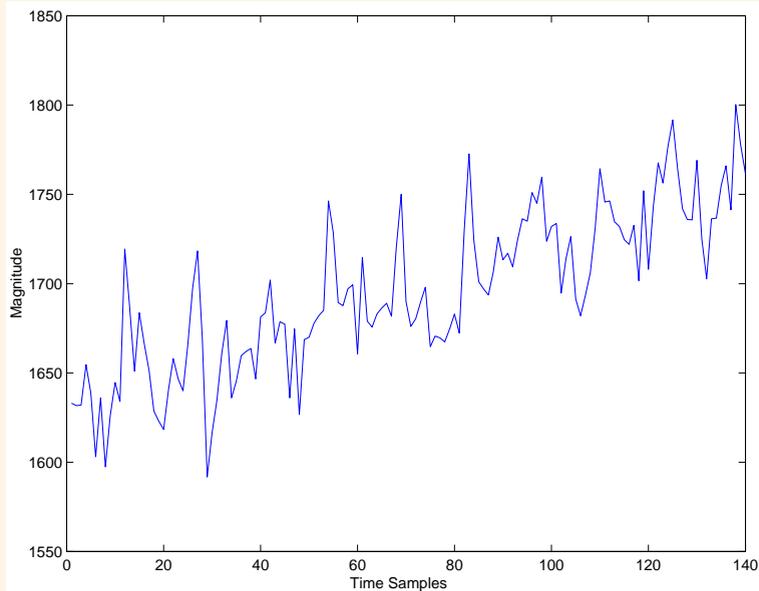
Visual stimulus: activation maps



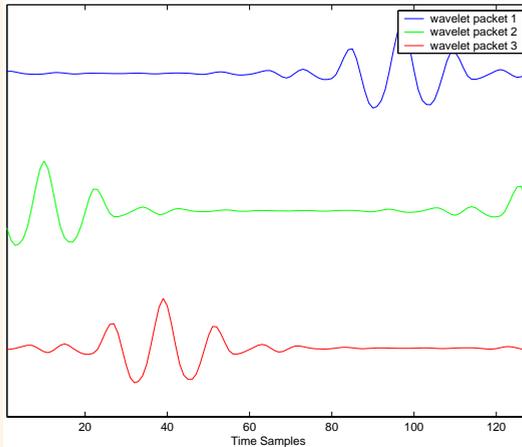
Activation maps obtained with our method

Experiments : in vivo data

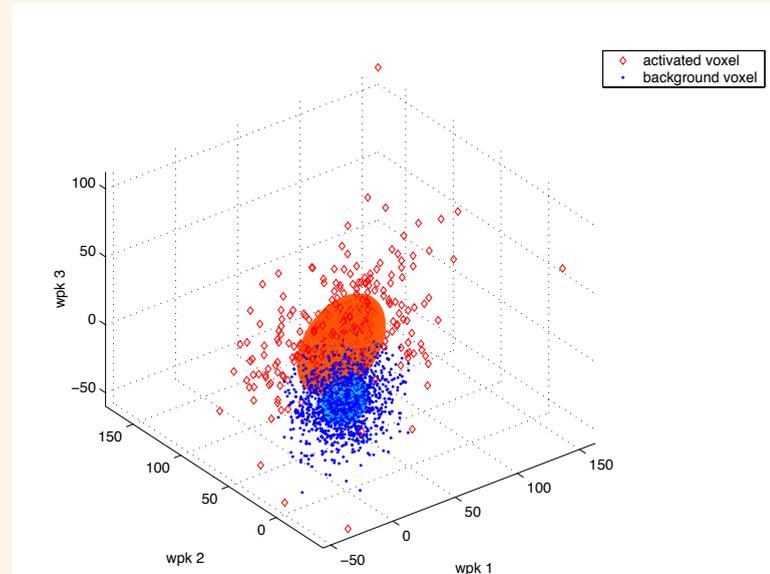
- visual-mental imagery : random presentation



Experiments : in vivo data

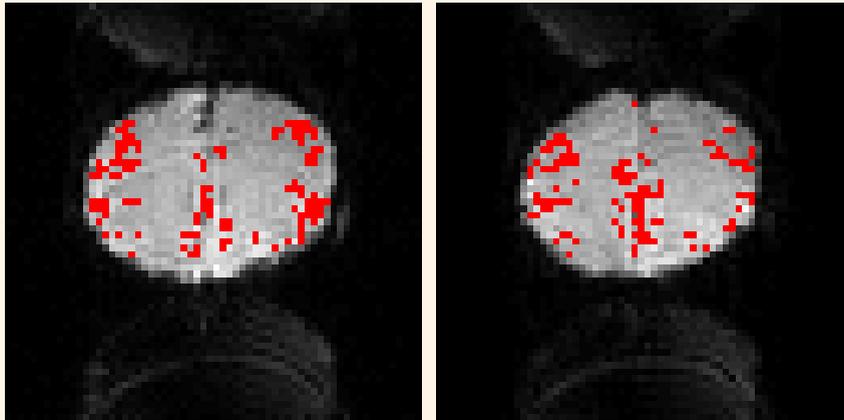


Projections ($K=3$)

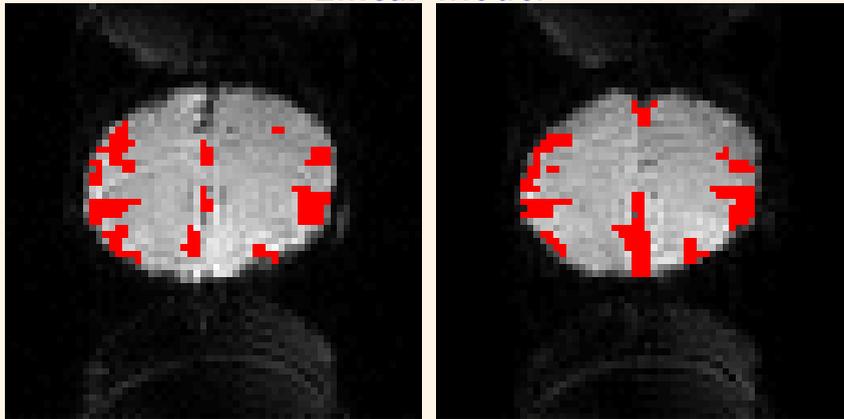


background (blue) and
activated (red) time series

Visual/Mental Imagery: activation maps



Linear model



Our method

Conclusion

- projection of the fMRI time series on a low dimensional subspace :
 - reveal the presence of activated time series.
 - probability distribution of the projections (coefficients) :
finite mixture of multivariate Gaussian densities
 - estimate the parameters of the mixture, number of components, and interpret their physiological roles.
- spatial prior : activated voxels should be spatially clustered

Acknowledgment

- fMRI dataset collected by Dr. Jody Tanabe,

References

- [Baumgartner et al., 1998] Baumgartner, R., Windischberger, C., and Moser, E. (1998). Quantification in functional magnetic resonance imaging : fuzzy clustering vs. correlation analysis. *Magnetic Resonance Imaging*, 16:115–125.
- [B.B.Biswal and Ulmer, 1999] B.B.Biswal and Ulmer, J. (1999). Blind source separation of multiple signal sources of fMRI data sets using independent component analysis. *Journal of Computer Assisted Tomography*, 23(3):265–271.
- [Chen et al., 2003] Chen, C., Tyler, C., and Baseler, H. (2003). Statistical properties of BOLD magnetic resonance activity in the human brain. *NeuroImage*, 20:1069–1109.
- [Fadili and Bullmore, 2002] Fadili, J. and Bullmore, E. (2002). Wavelet-generalized least squares : a new BLU estimator of linear regression models with $1/f$ errors. *NeuroImage*, 15:217–232.
- [Friston et al., 1995] Friston, K., Holmes, A., Worsley, K., Poline, J., Frith, C., and Frackowiak, R. (1995). Statistical parametric maps in functional imaging: A general linear approach. *Human Brain Mapping*, 2:189–210.
- [Friston et al., 1998] Friston, K., Josephs, O., Rees, G., and Turner, R. (1998). Nonlinear event-related responses in fMRI. *Magn. Reson. Med*, 39:41–52.
- [Gabbay et al., 2000] Gabbay, M., Brennan, C., Kaplan, E., and Sirovich, L. (2000). A principal components-based method for the detection of neuronal activity maps: application to optical imaging. *NeuroImage*, 11:313–325.
- [Genovese, 2000] Genovese, C. (2000). A Bayesian time-course model for functional magnetic resonance imaging data. *Journal of the American Statistical Association*, 95, 451:691–719.
- [Glover, 1999] Glover, G. (1999). Deconvolution of impulse response in event-related bold fMRI. *NeuroImage*, (9):416–429.
- [Golay et al., 1998] Golay, X., Kollias, S., Stoll, G., Meier, D., Valavanis, A., and Boesiger, P. (1998). A new correlation-based fuzzy logic clustering algorithm for fMRI. *Magnetic Resonance in Medicine*, 40:249–260.
- [Lai and Fang, 1999] Lai, S. and Fang, M. (1999). A novel local PCA-based method for detecting activation signals in fMRI. *Magnetic Resonance Imaging*, 17:827–836.

- [Lange and Zeger, 1997] Lange, N. and Zeger, S. (1997). Non-linear Fourier time series analysis for human brain mapping by functional magnetic resonance imaging. *Appl. Statist.*, 46(1):1–29.
- [McKeown, 2000] McKeown, M. (2000). Detection of consistently task-related activations in fMRI data with hybrid independent component analysis. *NeuroImage*, (11):24–35.
- [Meyer and Chinrungrueng, 2004] Meyer, F. and Chinrungrueng, J. (2004). Spatiotemporal clustering of fMRI time series in the spectral domain. *Medical Image Analysis*.
- [Meyer and Shen, 2004] Meyer, F. and Shen, X. (2004). Multiscale analysis of fmri data with mixture of gaussian densities. submitted to *IEEE Transactions on Medical Imaging*.
- [Miller et al., 2001] Miller, K., Luh, W., Liu, T., Martinez, A., Obata, T., Wong, E., Frank, L., and Buxton, R. (2001). Nonlinear temporal dynamics of the cerebral blood flow response. *Human Brain Mapping*, 13:1–12.
- [Rees et al., 1997] Rees, G., Howseman, A., Josephs, O., Frith, C., Friston, K., Frackowiak, R., and Turner, R. (1997). Characterizing the relationship between BOLD contrast and regional cerebral blood flow measurements by varying the stimulus presentation rate. *Human Brain Mapping*, 6:270–278.
- [Vanzetta and Grinvald, 1999] Vanzetta, I. and Grinvald, A. (1999). Increased cortical oxidative metabolism due to sensory stimulation: implications for functional brain imaging. *Science*, 286:1555–8.
- [Vazquez and Noll, 1998] Vazquez, A. and Noll, D. (1998). Nonlinear aspects of the BOLD response in functional MRI. *Human Brain Mapping*, 7:108–118.
- [Zarahn et al., 1997] Zarahn, E., Aguire, G., and D'Esposito, M. (1997). Empirical analysis of fMRI statistics : I. Spatially unsmoothed data collected under null hypothesis conditons. *Neuroimage*, 5:179–197.