# Imaging with the Helmholtz equation

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### Ultrasound Tomography





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### Kaczmarz with plane wave stacking in medical imaging



original

reconstruction

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Computing time <1 minute on a 3Ghz double processor PC

### Rays for the SLC breast phantom

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Role of parameter k:

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i) k determines the resolution  $\lambda=2\pi/k$ 

ii) k large makes it difficult to solve the Helmholtz equation numerically

### Usual treatment by X-ray transform: For $\gamma r \sup |f(x)| < \lambda \qquad \lambda = 2\pi/k$ |x| < rf(x) = 0 for |x| > rwe have $u(x) \approx \frac{k}{2i} \int f(x + se_3) ds$

# Goal of this talk: Exact (iterative) solution without any approximation, such as Born, Rytov, WKB,...

#### Initial Value Problem for the Helmholtz Equation

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 $x_1$ 

$$\frac{\partial^2 u}{\partial x_1^2} + \frac{\partial^2 u}{\partial x_2^2} + k^2 u = 0 \qquad u(x_1, 0) = u_0(x_1), \ \frac{\partial u}{\partial x_2}(x_1, 0) = u_1(x_1)$$

Fourier transform with respect to  $x_1$ :  $\hat{u}(\xi_1, x_2) = (2\pi)^{-1/2} \int \exp(-ix_1\xi_1)u(x_1, x_2)dx_1$ 

Ordinary differential equation in  $x_2$ :  $\frac{d^2 \hat{u}(\xi_1, x_2)}{dx_2^2} + (k^2 - \xi_1^2) \hat{u}(\xi_1, x_2) = 0$ Cauchy data

 $x_2$ 

Solution:

$$\hat{u}(\xi_{1}, x_{2}) = \hat{u}_{0}(\xi_{1})\cos(\kappa(\xi_{1})x_{2}) + \frac{\hat{u}_{1}(\xi_{1})}{\kappa(\xi_{1})}\sin(\kappa(\xi_{1})x_{2}), \ \kappa(\xi_{1}) = \sqrt{k^{2} - \xi_{1}^{2}}$$
  
Stable as long as  $\xi_{1}^{2} \le k^{2}$ 

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# Stability estimates for the Cauchy problem of the inhomogeneous Helmholtz equation

x'

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 $X_1$ 

 $X_n$ 

Cauchy data

$$\Delta u + k^2 (1+f)u = r, \quad x_n > 0, \quad f \ge 1 + m_1, \ m_1 > -1$$

$$u(x',0) = 0, \quad \frac{\partial u(x',0)}{\partial x_n} = 0, \quad x' \in \mathbb{R}^{n-1}$$

 $u_{\kappa}$  = low pass filtered (in x') version with cut - off  $\kappa$  of u

$$\|u_{\kappa\vartheta}(x',x_n)\|_{L^2(R^{n-1})} \le \frac{c(x_n)}{\kappa\vartheta} \|r\|_{L^2(R^{n-1}\times[0,x_n])}, \quad \kappa = k(1+m_1), \quad 0 < \vartheta < 1$$

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#### Stable marching for the Helmholtz equation

Compute a preliminary value  $U_{l,j+1}$  from  $-4u_{l,j} + U_{l,j+1} + u_{l,j-1} + u_{l+1,j} + u_{l-1,j} + h^2 k^2 (1 + f_{l,j}) = 0$ 

Compute  $u_{l,j+1}$  by low pass filtering of  $U_{l,j+1}$ with respect to l



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Exact (finite difference time domain, followed by Fourier transform)

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 $f(x) = (1 - |x|^2)_+$ 

Initial value technique





### Kaczmarz' method for Helmholtz equation in frequency domain

Define  $R_{\theta}(f) = u|_{\Gamma_{\theta}^{+}}$  where *u* solution of

$$\Delta u + k^2 (1+f)u = 0, \ u = g_{\theta}^-, \ \frac{\partial u}{\partial \theta} = \frac{\partial g_{\theta}^-}{\partial \theta} \text{ on } \Gamma_{\theta}^-$$

Solve  $R_{\theta}(f) = g_{\theta}$  for all measured directions  $\theta$  iteratively:

Update:  $f \leftarrow f - \alpha (R'_{\theta}(f))^* (R_{\theta}(f) - g_{\theta})$ 

Evalutation of  $(R'_{\theta}(f))^* r$ :  $(R'_{\theta}(f))^* r = \overline{z}\overline{u}$ 

 $\Delta z + k^2 (1+f)z = 0$  $z = 0, \ \frac{\partial z}{\partial v} = \overline{r} \text{ on } \Gamma_{\theta}^+$ 

time reversal backpropagation backprojecton adjoint differentiation migration  $\langle 1 | 1 \rangle$ 

Example for Kaczmarz' method for simple object R R  $\mathfrak{I}$  $\mathfrak{I}$ 32 superimposed backpropagated fields object 16 superimposed backpropagated fields scattered field .2 time reversed backpropagated field data

Original wavelength

Reconstruction from waves (full range)

Reconstruction from line integrals (full range)



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### Data



range 120°







### Conclusions

Imaging from waves is possible Algorithms roughly as efficient as ART in ET Resolution corresponds to wavelength Limited angle for waves easier than for ET